

## **Reliability of Orthostatic Beat-to-Beat Blood Pressure Tests: Implications for Population and Clinical Studies**

C Finucane<sup>1</sup>, GM Savva<sup>3</sup>, RA Kenny<sup>2</sup>

<sup>1</sup>Dept. of Medical Physics and Bioengineering, Mercer's Institute for Successful Ageing, St. James's Hospital, Dublin, Ireland.

<sup>2</sup>The Irish Longitudinal Study on Ageing (TILDA), Department of Medical Gerontology, Trinity College Dublin, Ireland.

<sup>3</sup>School of Health Sciences, University of East Anglia, Norwich Research Park, Norwich, NR4 7TJ. United Kingdom.

### **Corresponding Address:**

Ciarán Finucane, Dept. of Medical Physics, Mercer's Institute for Successful Ageing, St. James's Hospital, Dublin, Ireland.

E-mail: [cfinucane@stjames.ie](mailto:cfinucane@stjames.ie)

Telephone: 00 353 1 410 2645

## **Abstract**

### **Objective**

To assess the test-retest reliability of orthostatic beat-to-beat blood pressure responses to active standing and related clinical definitions of orthostatic hypotension.

### **Methods**

A random sample of community dwelling older adults from the pan-European Survey of Health, Ageing and Retirement in Europe, Ireland underwent a health assessment which mimicked that of the Irish Longitudinal Study on Ageing. An active stand test was performed using continuous blood pressure measurements. Participants attended a repeat assessment 4-12 weeks after the initial measurement. A mixed-effects regression model estimated the reliability and minimum detectable change while controlling for fixed observer and time of day effects.

### **Results**

A total of 125 individuals underwent repeat assessment (mean age  $66.2 \pm 7.5$ ; 55.6% women). Mean time between visits was  $84.3 \pm 23.3$  days. There was no significant mean difference in heart rate or blood pressure recovery variables between the first and repeat assessments. Minimum detectable change was noted for changes from resting values in systolic blood pressure (26.4 mmHg) and diastolic blood pressure (13.7 mmHg) at 110 seconds and for changes in heart rate (10.9 bpm) from resting values at 30 seconds after standing. Intra-class correlation values ranged from 0.47 for nadir values to 0.80 for heart rate and systolic blood pressure values measured 110 seconds after standing.

### **Conclusion**

Continuous orthostatic beat-to-beat blood pressure and related clinical definitions show moderate reliability and substantial natural variation over a 4-12 week period. Understanding variation in measures is essential for study design or estimating the effects of orthostatic hypotension, while clinically it can be used when evaluating longer term treatment effects.

## Introduction

Orthostatic blood pressure (BP) responses are used to identify patients with orthostatic hypotension who are at risk of syncope, falls and autonomic dysfunction[1]. Traditionally, auscultatory or oscillometric BP measurement methods have been employed[2]. Over the past twenty years emerging clinical and epidemiological practice has shifted towards the use of continuous beat-to-beat BP(CBP) measurements[3]. Impairments in CBP responses are related to increased levels of frailty[4], cognitive impairment[5], and falls risk[6] in cross-sectional and longitudinal studies.

Understanding the reliability of CBP measurements is important in all applications of these measures. Numerous approaches for characterising altered CBP behaviour[7] are suggested in the literature e.g. initial orthostatic hypotension[8], classical orthostatic hypotension (OH)[3], impaired BP stabilisation [9], and morphological approaches[6]. Given that traditional BP measurements have considerable intra- and inter-individual variability[10] and intra-observer effects[11] we hypothesize that CBP are similarly affected.

Information on measurement error for CBP is important for clinical practice and research studies. Clinical diagnoses require repeatable and robust biomarkers with well characterised intra- and inter- individual variability [11], while in research, knowledge of measurement error is used in power calculations, to select outcome measures and to reduce errors associated with incomplete correction of confounding and regression dilution bias [12].

In this paper we focus on the medium term (4-12 weeks) reliability of active stand responses and related classifications of OH using CBP approaches in a population study of adults aged over 50 years. Bias, standard error of measurement (SEM), minimal detectable change

(MDC) between measurements, intra-class correlation coefficients (ICC) and kappa statistics are reported.

## **Methods**

### **Study population**

Participants for this study were recruited from a random sample of older adults ( $n \approx 1100$ ) aged over 50 living in Ireland who previously took part in the pan-European Survey of Health, Ageing and Retirement in Europe (SHARE), Ireland between 2006 and 2007[15]. These individuals were invited to take part in a health assessment in 2011 which mimicked that of the Irish Longitudinal Study on Ageing (TILDA) and included an active stand test [13][14]. A short-form version of the TILDA computer aided personal interview (CAPI) was administered during this assessment to provide demographic and self-reported health and socioeconomic information.

To examine the repeatability of outcome variables participants attended for a repeat health assessment approximately 4-12 weeks after the baseline measurement. To control for the effects of time-of-day and observer on the outcome variables participants were randomly assigned to have their health assessment performed either in the morning (AM: 9.30am) or afternoon (PM: 2:00pm) and to be assessed by 1 of 2 research nurses. Ethical approval was obtained from Trinity College Dublin ethics committee and all respondents provided signed informed consent prior to participation. All experimental procedures adhered to the Declaration of Helsinki.

### **Inclusion and Exclusion Criteria**

This nationally representative sample was constructed using the RANSAM framework [14] using a 2-stage clustered sampling process using the Irish Geodirectory as the sampling frame. The Irish Geodirectory is a comprehensive listing of all addresses in the Republic of Ireland. These addresses were assessed for eligibility, and members of eligible households aged  $\geq 50$  years were canvassed to participate in the study. The  $n \approx 1100$  individuals that participated in the original SHARE study were subsequently invited to participate in the health assessment as described above. Patients with specific autonomic dysfunction were not excluded from the study, however those who lacked capacity to consent to the study or were living in institutional care were excluded.

### **Continuous Orthostatic Blood Pressure Measurement**

CBP responses to orthostasis were measured using the volume clamp method (Finometer<sup>®</sup>, Finapres Medical Systems, Arnhem, The Netherlands) as previously described [16][3]. Measurements were performed in a quiet, temperate room (21-23°C). Participants rested in the supine position for 10 minutes and were then instructed to stand. Assistance to mobilise was provided as required. Participants stood while systolic BP (SBP), diastolic BP (DBP), and heart rate (HR) were monitored for 2.5 minutes with subjects reporting symptoms of dizziness, light-headedness or unsteadiness during the stand (coded as orthostatic symptoms). The measurement hand (left) was maintained by the participant's side throughout the period of measurement. The height correction unit was used to correct for any hydrostatic offsets introduced during change of position [3,16]. The Physiocal<sup>®</sup> system remained on during the supine rest period and was switched off just prior to the stand. This identical protocol was repeated on the second health assessment visit by the assigned research nurse. The role of the observing research nurse was to guide participants

throughout the protocol according to a standard operating procedure. Data analyses were performed independently of the observer [16].

### **Data Analysis of CBP Records**

Raw CBP data was automatically processed to reject artefacts, and perform moving average filtering and BP waveform feature extraction [16]. A 2-second moving average filter was applied to the raw CBP to allow nadir and peak CBP and HR values to be extracted with a high time resolution while also minimising noise. A moving average filter (+/-5 seconds around each reported time point) was applied to the raw CBP e.g. the filtered value at 60 seconds is a weighted mean of the values occurring in the window from 55-65 secs. This data was used to capture the recovery trends as per previous work [3,16] while balancing noise reduction, the data set size for epidemiological samples and falls risk prediction. The following features were automatically extracted [3][16]: *Supine SBP, DBP and HR*: Values of SBP ( $SBP_B$ ), DBP ( $DBP_B$ ) and HR ( $HR_B$ ) defined as the average of supine data occurring -60 to -30 seconds prior to standing; *Systolic BP and Diastolic BP Nadirs*: Minimum SBP or DBP value occurring within 30 seconds of standing denoted  $SBP_{Nadir}$  and  $DBP_{Nadir}$ ; *Peak HR*: *Maximum heart rate ( $HR_{Peak}$ ) after standing was defined given its association with ageing [3] and autonomic dysfunction [17]*; *Recovery values at specified time intervals*: SBP, DBP, and HR values at takes on values 30, 60, 90 and 110 seconds post-stand. These values are denoted  $SBP(t)$ ,  $DBP(t)$ , and  $HR(t)$  where t is time in seconds after standing; *Delta values at specified time intervals*: Change in SBP, DBP, and HR values from supine values. These values are denoted  $\Delta SBP(t)$ ,  $\Delta DBP(t)$ , and  $\Delta HR(t)$  where t is time in seconds after standing and takes on values 30, 60, 90 and 110 seconds; *Impaired orthostatic BP stabilisation  $OH(t)$*  was defined as failure to return to within  $SBP \geq 20\text{mmHg}$  and/or  $DBP \geq 10\text{mmHg}$  of supine levels at t seconds after standing where t is time in seconds after standing and takes on values 30 to 90

seconds in 30-second intervals. An additional analysis examined the effect of including a modified threshold of 30mmHg SBP drop in those with supine systolic hypertension >160mmHg. *Sustained tachycardia* was defined as a sustained HR increase of >30bpm or a HR of 120bpm at all time points after standing.

### **Participant Characteristics**

The following characteristics were recorded: age (years), gender, height (cm), body mass index (BMI–kg/m<sup>2</sup>), mean gait speed (cm/sec), dominant hand grip strength (kg), history of fractures, faints, falls, a doctor’s diagnosis of heart attack, hypertension, high cholesterol, stroke, diabetes, atrial fibrillation, arthritis, osteoporosis. Medication use was quantified to capture the number of medications taken, those on antihypertensives and polypharmacy (taking ≥5 medications). To assess global cognition the Montreal Cognitive Assessment (MOCA) was administered [18], with mental health assessed using the 8-item Centre for Epidemiological Studies Depression (CES-D) scale [19] [13].

### **Statistical Analyses**

Analyses were performed using Stata (ver.12). Paired t-tests for continuous variables were applied to assess univariate mean differences across time points for each measure (See Table 2). For each continuous variable a linear mixed-effects model (Table 3) was estimated including random effect of participant and fixed effects of time-of-day, and observer effects. From the model the standard deviation of the between participant ( $SD_{between}$ ; standard deviation of the random effect) and within participant variation ( $SD_{within}$ ; residual standard deviation) were extracted. ICC, the proportion of variability explained by between-individual differences, was estimated as  $ICC = SD_{between}^2 / (SD_{within}^2 + SD_{between}^2)$  (See Table 3). A False Discovery rate approach was used to control for multiple testing with a corrected significance level of  $P = 0.0015$  [20] for statistical significance. Bland-Altman plots

(Supplementary Figure 1-3) were used to estimate the mean difference between repeated measures (bias) and the MDC for each continuous measure. The MDC reflects the maximum difference between two occasions that could be attributed to chance within the same individual given the estimated within-person variability for each measure. MDC is estimated by  $MDC = SD_{Within} \times \sqrt{2} \times Z$  where  $Z = 1.96$  for the 95% MDC. The agreement across time points of the following binary classifications: OH, OH(t) (at all time-points  $t=10,20,\dots,110$  seconds after standing) and sustained tachycardia was reported using Cohen's Kappa statistic.

## **Results**

### **Sample**

Data from 125 participants aged  $66.2 \pm 7.5$  years old of whom 55.6% are women were available for analysis with five participants without a complete active stand dataset. 82 (65.6%) participants were allocated a different observer (Observer 1 versus Observer 2), while 57 (45.6%) were assigned a different time of day (AM versus PM) for the second visit. The mean time between visits was  $84.3 \pm 23.3$  days. Participant characteristics are detailed in Table 1.

### **Reliability of CBP Measurements**

After correcting for multiple testing, univariate analysis showed that some absolute measures of BP were lower at repeat compared to baseline. This, however, resulted in no substantial mean differences in BP recovery between the baseline and repeat measurement, where only a few statistical differences were found. Mean HR and HR recovery were similar



in the baseline and repeat assessments (Table 2). We found the same results after multivariate analysis with time-of-day and observer as covariates (Table 3).

Substantial within-person variation was noted across all absolute measures of SBP, DBP and HR. These values had (by conventional cut-offs) moderate to high repeatability with ICC values ranging from 0.6 to 0.8, with HR more reliable than BP values.

The repeatability of the baseline corrected parameters were lower, with similar magnitudes of variation within and between individuals leading to moderate ICC values ranging of 0.4-0.7.

The MDC for absolute SBP ranged from 32.7mmHg to 39.4mmHg. The MDC values for absolute DBP are smaller and ranged from 15.9mmHg at 110 seconds after standing to 20.2mmHg at the nadir. HR MDC values ranged from 12.7bpm to 16.7bpm. MDC values for values corrected for supine resting values were marginally improved (Table 3). Figures 1-3 depict the Bland-Altman plots for these relationships.

### **Reliability of Orthostatic Hypotension and Related Classifications**

Classical OH ( $\kappa=0.21$ ;  $P=0.009$ ), OH(t) demonstrated low to moderate agreement across repeated measurements with the reliability of OH(t) highest at 50 seconds after standing ( $\kappa=0.40$ ;  $P<0.0001$ ) (Table 4). For example, although 16 out of 125 participants were classified at both the baseline assessment and at the repeat, only 5 of these were classified with OH on both occasions.

Additional analysis indicated that the reliability of OH definition was not sensitive to the effect of changing the diagnostic threshold to 30mmHg in those with supine hypertension >160mmHg.

## Discussion

Continuous BP and HR measurements (and commonly derived clinical measures e.g. OH) during standing have low to moderate levels of reliability (ICC=0.46-0.80 for continuous measures,  $\kappa$ =0.21–0.40 for binary classifications) and MDC over a 4-12 week period. While many absolute BP measures were lower during the repeat visit, there was less systematic difference in measures of BP recovery.

The mean values of SBP, DBP, HR,  $\Delta$ SBP,  $\Delta$ DBP,  $\Delta$ HR are relatively stable across a 4-12 week period. HR values are the most reliable with DBP being the least reliable. From the Bland-Altman plots (Supplementary Figure) it is evident that the MDC are wide and range from 25-40mmHg for SBP/ $\Delta$ SBP, 11-16mmHg for DBP/ $\Delta$ DBP and 12-16bpm for HR/ $\Delta$ HR measures.

Clinicians should be aware of the MDC in these measures when assessing the effect of interventions or the progression of patients. Owing to the natural variation and day-to-day changes in factors that affect BP, 95% of patients would be expected to exhibit changes within the 95% MDC by chance alone when two measures taken at different times are compared.

From a research perspective, knowledge of between and within-person variability will assist in performing power calculations, and reducing bias associated with misclassified exposure (otherwise called predictor or independent variables) or confounding variables. Regression dilution bias occurs when exposure variables are measured with error, and causes underestimation of effects. This bias can be corrected using the reliability information we report here [12]. The degree of dilution is determined by the reliability of the exposure measurement, given here by ICC ranging from 0 to 1. For example an uncorrected estimate,

$\beta = -0.15$ , of the association between increasing  $\Delta\text{SBP}(30)$  and measures of global cognition is biased downwards if an unreliable measurement of  $\Delta\text{SBP}(30)$  is used. This can be corrected by applying the correction formula  $\beta_{\text{corrected}} = \beta / \text{ICC}$ . This gives a corrected coefficient of  $\beta_{\text{corrected}} = -0.25$ , where  $\text{ICC} = 0.59$  is reported in Table 3. Our findings are therefore important to those estimating the effects of impaired BP recovery on future health outcomes. More generally, measurement error in confounding variables can also lead to false positive effects, because confounding control for such variables will be incomplete if unreliable measures are used. Procedures such as errors-in-variables regression can produce unbiased estimates, but rely on knowing the reliability or the within-person standard deviation to correct these effects. Hence our estimates are also important to those using such measures as confounding variables [12].

The reported variability here is comparable to previous reports of autonomic function and BP measures [21,22] and is likely physiological in origin [23]. It is well-known that SBP, DBP and HR fluctuate considerably over a broad range of time scales i.e. diurnal to seasonal [10][24]. These fluctuations are thought to arise from internal and external sources including changes in neurohormonal activity [25], circulating volume [26], changes in sympathetic and parasympathetic activity [8], and environmental effects [11]. Furthermore the active stand response is under the influence of a number of additional factors including self-selected speed of standing, muscle pump activation [27], movement artefact [16], time of day [28] and other experiment effects (e.g. observer) which are likely to further effect the repeatability of measurements. Previous studies have noted that orthostatic BP measurements have relatively poor reproducibility [29][30], with the reproducibility thought to be higher in those with neurogenic OH[31]. Others have also noted low levels of

agreement in OH definitions (kappa 0.17–0.32) based on active stands performed at the same time on different days [32], suggesting that at least in this relatively healthy population, OH can be transient for a numbers of people.

### **Strengths and Limitations**

A number of limitations are worth noting in our study. Underlying physiological changes e.g. hydration status over a 4-12 week period may have occurred, which may account for some of the within individual variability detected. No restrictions were placed on participants in terms of exercise, food intake, medications all of which may contribute to measurement variability. Repeating this study over a shorter-time frame in a more controlled environment, with the inclusion of same day repeated measurements could lead to higher estimates of reliability, but our findings reflect the variation likely to be observed in real world settings. The presence of orthostatic symptoms was noted however the severity and type was not quantified nor was the reliability of initial orthostatic hypotension since [33]. Although we recognise the duration of the stand was shorter than advised by AAS consensus criteria, this was for a number of reasons: the challenges of a large epidemiological study require a trade-off between sample representativeness and length of time to conduct individual tests; based on an initial pilot study 95% of the population had recovered by 120 seconds; the duration of the data reported (110 seconds) was chosen to minimise missing data and end effects which influence the moving average filtering process [3].

This study has a number of significant strengths. A community representative sample was studied allowing our results to be generalised to community dwelling individuals. Given the prevalence of OH (12.8%), sustained tachycardia on standing (5.6%) and diabetes (6.4%) in this sample, it is also captures those with autonomic dysfunction. A dedicated sample would

be required to focus on specific autonomic disorders e.g. diabetic autonomic neuropathy. However our findings suggest that within-person standard deviation is not linked to absolute values of BP recovery, and so there is no evidence that our estimates of within-person standard deviation would not be applicable in this group although it would be interesting to examine these relationships in individuals with type 2 diabetes or hypertension [34]. A comprehensive battery of physical, cognitive and mental health measures was obtained, alongside socioeconomic and health utilisation metrics. All measures were collected using internationally standardised protocols.

## **Conclusion**

Continuous BP and HR measurements and related clinical definitions of OH during standing show moderate reliability and substantial natural variation over a 4-12 week period. Understanding variation in measures is essential for researchers designing studies or estimating the effects of OH, while in clinical settings reliability statistics should be considered when evaluating longer term treatment effects.

## **Acknowledgements**

The authors would like to acknowledge the contribution of the participants, members of the TILDA and SHARE teams. Funding for TILDA was received from the Atlantic Philanthropies, the Irish Government, and Irish Life plc. The TILDA-SHARE collaboration was funded by a National Institute for Ageing grant number R21 AG040387.

## **Disclosures**

On behalf of all authors, the corresponding author states that there is no conflict of interest.

## References

1. Moya et al. Guidelines for the diagnosis and management of syncope (version 2009): The Task Force for the Diagnosis and Management of Syncope of the European Society of Cardiology (ESC). *European Heart Journal*. 2009 Nov 1;30(21):2631–71.
2. Freeman R, Wieling W, Axelrod FB, Benditt DG, Benarroch E, Biaggioni I, et al. Consensus statement on the definition of orthostatic hypotension, neurally mediated syncope and the postural tachycardia syndrome. *Clin Auton Res*. 2011 Apr;21(2):69–72.
3. Finucane C, Connell MO, Fan CW, Soraghan C, Cronin H, Kenny RA. The population distribution of orthostatic blood pressure responses in older community dwelling adults: Is 40 s the new 20/10? *Autonomic Neuroscience*. 2013 Oct;177(2):311.
4. Romero-Ortuno R, Cogan L, O'Shea D, Lawlor BA, Kenny RA. Orthostatic haemodynamics may be impaired in frailty. *Age Ageing*. 2011 Sep 1;40(5):576–83.
5. Frewen J, Finucane C, Savva GM, Boyle G, Kenny RA. Orthostatic Hypotension Is Associated With Lower Cognitive Performance in Adults Aged 50 Plus With Supine Hypertension. *J Gerontol A Biol Sci Med Sci*. 2014 Jul 1;69(7):878–85.
6. Romero-Ortuno R, O'Connell MD, Finucane C, Soraghan C, Fan CW, Kenny RA. Insights into the clinical management of the syndrome of supine hypertension – orthostatic hypotension (SH-OH): The Irish Longitudinal Study on Ageing (TILDA). *BMC Geriatrics*. 2013 Jul 15;13(1):73.

7. Frith J, Newton JL, Parry SW. Measuring and defining orthostatic hypotension in the older person. *Age Ageing*. 2014 Mar 1;43(2):168–70.
8. Wieling W, Krediet CTP, van Dijk N, Linzer M, Tschakovsky ME. Initial orthostatic hypotension: review of a forgotten condition. *Clin Sci*. 2007 Feb;112(3):157–65.
9. Lagro J, Laurensen NCW, Schalk BWM, Schoon Y, Claassen JAHR, Rikkert MGMO. Diastolic blood pressure drop after standing as a clinical sign for increased mortality in older falls clinic patients: *Journal of Hypertension*. 2012 Jun;30(6):1195–202.
10. Schwartz GL, Turner ST, Moore JH, Sing CF. Effect of time of day on intraindividual variability in ambulatory blood pressure. *Am J Hypertens*. 2000 Nov;13(11):1203–9.
11. O'Brien E, Waeber B, Parati G, Staessen J, Myers MG. Blood pressure measuring devices: recommendations of the European Society of Hypertension. *BMJ*. 2001 Mar 3;322(7285):531–6.
12. Hutcheon JA, Chioloro A, Hanley JA. Random measurement error and regression dilution bias. *BMJ*. 2010 Jun 23;340(jun23 2):c2289–c2289.
13. Cronin H, O'Regan C, Finucane C, Kearney P, Kenny RA. Health and Aging: Development of The Irish Longitudinal Study on Ageing Health Assessment. *J Am Geriatr Soc*. 2013 May 1;61:S269–S278.
14. Whelan BJ, Savva GM. Design and Methodology of The Irish Longitudinal Study on Ageing. *J Am Geriatr Soc*. 2013 May 1;61:S265–S268.

15. Delaney L, Harmon C, Kelleher C, Kennedy J, Gannon B, O'Shea E. SHARE Ireland first results [Internet]. University College Dublin. Geary Institute; 2008 [cited 2014 Sep 30]. Available from: <http://researchrepository.ucd.ie/handle/10197/1204>
16. Soraghan CJ, Fan CW, Hayakawa T, Cronin H, Foran T, Boyle G, et al. TILDA Signal Processing Framework (SPF) for the analysis of BP responses to standing in epidemiological and clinical studies. 2014 IEEE-EMBS International Conference on Biomedical and Health Informatics (BHI). 2014. p. 793–6.
17. Wieling W, van Brederode JF, de Rijk LG, Borst C, Dunning AJ. Reflex control of heart rate in normal subjects in relation to age: a data base for cardiac vagal neuropathy. *Diabetologia*. 1982 Mar;22(3): 163-6.
18. Nasreddine ZS, Phillips NA, Bédirian V, Charbonneau S, Whitehead V, Collin I, et al. The Montreal Cognitive Assessment, MoCA: a brief screening tool for mild cognitive impairment. *J Am Geriatr Soc*. 2005 Apr;53(4):695–9.
19. Newson R, ALSPAC Study Team. Multiple-test procedures and smile plots. *The Stat Journal* 2003; 3(2), pp.109-132
20. Radloff LS. The CES-D Scale A Self-Report Depression Scale for Research in the General Population. *Applied Psychological Measurement*. 1977 Jun 1;1(3):385–401.
21. Hartwig MS, Cardoso SS, Hathaway DK, Gaber AO. Reliability and validity of cardiovascular and vasomotor autonomic function tests. *Diabetes Care*. 1994 Dec;17(12):1433–40.
22. Ziegler D, Laux G, Dannehl K, Spüler M, Mühlen H, Mayer P, et al. Assessment of Cardiovascular Autonomic Function: Age-related Normal Ranges and Reproducibility



of Spectral Analysis, Vector Analysis, and Standard Tests of Heart Rate Variation and Blood Pressure Responses. *Diabetic Medicine*. 1992 Mar 1;9(2):166–75.

23. Gabbett TJ, Gass GC. Reliability of orthostatic responses in healthy men aged between 65 and 75 years. *Exp Physiol*. 2005 Jul 1;90(4):587–92.
24. Mancia G, Bombelli M, Facchetti R, Madotto F, Corrao G, Trevano FQ, et al. Long-term prognostic value of blood pressure variability in the general population: results of the Pressioni Arteriose Monitorate e Loro Associazioni Study. *Hypertension*. 2007 Jun;49(6):1265–70.
25. Conway J, Boon N, Davies C, Jones JV, Sleight P. Neural and humoral mechanisms involved in blood pressure variability. *J Hypertens*. 1984 Apr;2(2):203–8.
26. Smith JJ, Porth CJ. Posture and the circulation: the age effect. *Exp Gerontol*. 1991;26(2-3):141–62.
27. Smit AAJ, Halliwill JR, Low PA, Wieling W. Pathophysiological basis of orthostatic hypotension in autonomic failure. *The Journal of Physiology*. 1999 Aug;519(1):1–10.
28. Fan CW, Savva GM, Finucane C, Cronin H, O'Regan C, Kenny RA. Factors affecting continuous beat-to-beat orthostatic blood pressure response in community-dwelling older adults. *Blood Press Monit*. 2012 Aug; 17(4):160-3. doi: 10.1097/MBP.0b013e328356821f.
29. Frith J. Diagnosing orthostatic hypotension: a narrative review of the evidence. *Br Med Bull*. 2015 Sep;115(1):123-34. doi: 10.1093/bmb/ldv025.

30. Naschitz JE, Rosner I. Orthostatic hypotension: framework of the syndrome. *Postgrad Med J* 2007;83:568–74.
31. Weiss A, Chagnac A, Beloosesky Y, et al. Orthostatic hypotension in the elderly: are the diagnostic criteria adequate? *J Hum Hypertens* 2004;18:301–05.
32. Belmin J, Abderrhamane M, Medjahed S, et al. Variability of blood pressure response to orthostatism and reproducibility of the diagnosis of orthostatic hypotension in elderly subjects. *J Gerontol A Biol Sci Med Sci* 2000;55:M667–71
33. van Wijnen VK, Harms MP, Go-Schön IK, Westerhof BE, Krediet CT, Stewart J, Wieling W. Initial orthostatic hypotension in teenagers and young adults. *Clin Auton Res*. 2016 Dec;26(6):441-449. Epub 2016 Sep 16.
34. Costa A, Bosone D, Ramusino MC, Ghiotto N, Guaschino E, Zoppi A, D'Angelo A, Fogari R. Twenty-four-hour blood pressure profile, orthostatic hypotension, and cardiac dysautonomia in elderly type 2 diabetic hypertensive patients. *Clin Auton Res*. 2016 Dec;26(6):433-439. Epub 2016 Sep 13.

**Table 1: Cohort characteristics.**

Age (Years), Mean (SD)	66.2 ±7.5
Gender (Male), % (N)	44.4 ±55
Height (cm), Mean (SD)	165.3 ± 10.2
Body Mass Index (kg/m <sup>2</sup> ), Mean (SD)	28.3 ± 4.1
<b>Cardiovascular Conditions</b>	
Heart Attack, % (N)	6.4 (8)
Hypertension, % (N)	39.2 (49)
High Cholesterol, % (N)	55.2 (69)
Stroke, % (N)	4.0 (5)
Diabetes, % (N)	6.4 (8)
Atrial Fibrillation, % (N)	2.4 (3)
<b>Other Relevant Medical History</b>	
Arthritis, % (N)	27.2 (34)
Osteoporosis, % (N)	14.4 (18)
History of Fractures, % (N)	16.0 (20)
History of Falls, % (N)	4.8 (6)
History of Fainting, % (N)	7.2 (9)
Orthostatic Symptoms, % (N)	25.6 (32)
<b>Physical Health measures</b>	
CES-D, Mean (SD)	4.3 ±3.8
MOCA, Mean (SD)	24.9 ±3.6
Gait speed (cm/sec), Mean (SD)	138 ±20.3
Grip strength dominant hand (kg), Mean (SD)	31.5 ±10.7
<b>Medication Use</b>	
Polypharmacy, % (N)	40.0 (50)
Antihypertensives, % (N)	41.6 (52)
Number of Medications, % (N)	4.3 (2.7)
<b>Cardiovascular Response to Standing</b>	
Classical Orthostatic Hypotension (OH), % (N)	12.8 (16)
Impaired orthostatic BP stabilisation, OH(40), % (N)	20.8 (26)
Sustained Tachycardia after Standing >30bpm or >120bpm <sup>a</sup> , % (N)	5.6 (7)
Sustained Tachycardia after Standing >30bpm or >120bpm without OH <sup>b</sup> , % (N)	0 (0)

**Table 1.** Cohort characteristics. History of fractures = ever fractured a hip, wrist or other bone; History of Falls = 1 or more falls in the past year; History of Syncope = 1 or more faints in the last year; MOCA Score= Montreal Cognitive Assessment; CES-D = Centre of Epidemiological Studies Depression Scale; BP = blood pressure; HR = heart rate; bpm = beats per minute. Sample size = 125. OH(40) = impaired blood pressure stabilisation defined as a drop of 20/10mmHg at 40 seconds after standing. OH = Orthostatic hypotension was defined as sustained failure of SBP or DBP to stabilise to within 20mmHg SBP or 10mmHg DBP of supine levels throughout the active stand from 60 to 110s after standing. <sup>a</sup> = no participants satisfied the >120bpm criteria. <sup>b</sup> = no participants satisfied both sustained tachycardia and sustained OH.

**Table 2: Univariate Repeatability of Active Stand Variables**

Variable	Baseline	Repeat	Variable	Baseline	Repeat
Supine SBP	143.3 ±23.4	140.9 ±21.5*	-	-	-
Supine DBP	74.1 ±9.2	73.5 ±8.6	-	-	-
Supine HR	65.5 ±9.3	64.8 ±9.5	-	-	-
SBP Nadir	108.9 ±22.3	104.0 ±22.1***	$\Delta$ SBP <sub>Nadir</sub>	34.4 ±15.7	36.9 ±16.6*
DBP Nadir	55.4 ±11.6	52.9 ±10.8***	$\Delta$ DBP <sub>Nadir</sub>	18.7 ±9.2	20.5 ±9.1*
HR Peak	84.3 ±12.0	83.5 ±11.7	$\Delta$ HR <sub>Peak</sub>	18.8 ±7.4	18.7 ±7.9
SBP(30)	140.6 ±23.6	135.5 ±24.6***	$\Delta$ SBP(30)	2.8 ±16.2	5.4 ±17.1*
DBP(30)	75.2 ±10.9	72.9 ±10.3**	$\Delta$ DBP(30)	-1.1 ±7.7	0.5 ±8.4*
HR(30)	72.0 ±12.1	71.8 ±11.8	$\Delta$ HR(30)	6.5 ±6.1	7.0 ±5.6
SBP(60)	138.9 ±24.3	134.3 ±25.8**	$\Delta$ SBP(60)	4.4 ±17.0	6.6 ±17.5
DBP(60)	75.0 ±11.0	72.6 ±11.0**	$\Delta$ DBP(60)	-0.9 ±7.6	0.8 ±8.3
HR(60)	73.3 ±11.7	73.2 ±11.1	$\Delta$ HR(60)	7.7 ±6.6	8.4 ±5.9
SBP(90)	141.8 ±23.8	137.6 ±25.0**	$\Delta$ SBP(90)	1.5 ±16.1	3.3 ±15.5
DBP(90)	76.3 ±11.0	73.9 ±10.6**	$\Delta$ DBP(90)	-2.2 ±7.1	-0.5 ±7.7*
HR(90)	72.7 ±11.9	73.4 ±10.8	$\Delta$ HR(90)	7.1 ±6.5	8.6 ±6.0
SBP(110)	141.3 ±24.5	137.9 ±24.6**	$\Delta$ SBP(110)	2.0 ±16.2	2.9 ±15.6
DBP(110)	75.8 ±11.0	74.2 ±10.3*	$\Delta$ DBP(110)	-1.8 ±7.1	-0.7 ±7.5
HR(110)	73.1 ±11.7	73.1 ±11.1	$\Delta$ HR(110)	7.5 ±6.4	8.2 ±5.9

**Table 2:** Univariate analysis of active stand variables reliability. Mean and standard deviation (SD) displayed. P value results from paired t-test of difference between means. All blood pressure values are reported in mmHg and heart rate values in beats per minute (bpm). SBP(t) = systolic BP at time t; DBP(t) = diastolic BP at time t; HR(t) = HR at time t.  $\Delta$  = values corrected for resting values. \* = P≤0.05; \*\*=P≤0.01;\*\*\* P≤0.0015.

**Table 3: Multivariate Reliability Statistics of Active Stand Variables**

Baseline vs Repeat			Reliability Statistics				Baseline vs Repeat			Reliability Statistics			
Variable	Diff. means	P Value	SD (Between participants)	SD (Within participants)	ICC	MDC	Variable	Diff. means	P Value	SD (Between participants)	SD (Within participants)	ICC	MDC
Supine SBP	3.0	0.069	18.6	12.3	0.70	34.1	-	-	-	-	-	-	-
Supine DBP	0.7	0.340	6.6	5.8	0.57	16.0	-	-	-	-	-	-	-
Supine HR	0.3	0.594	8.2	4.6	0.76	12.7	-	-	-	-	-	-	-
SBP Nadir	5.3	0.003**	17.7	13.2	0.64	36.7	$\Delta$ SBP <sub>Nadir</sub>	-2.4	0.080	12.4	10.2	0.64	28.2
DBP Nadir	2.5	0.010**	8.4	7.3	0.57	20.2	$\Delta$ DBP <sub>Nadir</sub>	-1.7	0.058	5.8	7.0	0.57	19.3
HR Peak	0.7	0.310	10.6	5.4	0.80	14.9	$\Delta$ HR <sub>Peak</sub>	-0.4	0.488	6.5	4.1	0.80	11.5
SBP(30)	5.4	0.002**	19.9	13.2	0.70	36.6	$\Delta$ SBP(30)	-2.4	0.082	12.6	10.5	0.60	29.1
DBP(30)	2.4	0.002**	8.6	6.0	0.67	16.7	$\Delta$ DBP(30)	-1.7	0.035*	5.4	5.9	0.41	16.5
HR(30)	-0.1	0.878	10.4	5.7	0.77	15.9	$\Delta$ HR(30)	0.4	0.421	4.2	3.9	0.71	10.9
SBP(60)	5.0	0.008**	20.4	14.2	0.67	39.4	$\Delta$ SBP(60)	-2.0	0.179	12.9	11.1	0.59	30.9
DBP(60)	2.5	0.003**	8.9	6.2	0.67	17.3	$\Delta$ DBP(60)	-1.7	0.018*	5.6	5.5	0.45	15.4
HR(60)	-0.1	0.937	9.6	6.0	0.72	16.7	$\Delta$ HR(60)	0.4	0.482	4.3	4.4	0.54	12.1
SBP(90)	4.7	0.005**	20.8	12.6	0.73	34.8	$\Delta$ SBP(90)	-1.7	0.243	11.4	10.7	0.57	29.5
DBP(90)	2.5	0.003**	8.6	6.3	0.65	17.4	$\Delta$ DBP(90)	-1.8	0.013*	5.0	5.4	0.51	15.0
HR(90)	-0.9	0.216	9.9	5.4	0.77	15.0	$\Delta$ HR(90)	1.2	0.030*	4.5	4.2	0.50	11.6
SBP(110)	4.0	0.012*	21.4	11.8	0.77	32.7	$\Delta$ SBP(110)	-0.9	0.481	12.5	9.5	0.54	26.4
DBP(110)	1.8	0.016*	8.8	5.7	0.70	15.9	$\Delta$ DBP(110)	-1.1	0.094	5.3	4.9	0.46	13.7
HR(110)	-0.3	0.720	10.0	5.4	0.77	15.0	$\Delta$ HR(110)	0.6	0.296	4.4	4.1	0.54	11.4

Multivariate Reliability Statistics of Active Stand Variables. Reliability summary statistics are also detailed where SD(Between participants) is the standard deviation between individuals, SD(Within participants) is the standard deviation within individuals, ICC is the intraclass correlation coefficient and MDC is the minimal detectable change. SBP(t) = systolic BP at time t; DBP(t) = diastolic BP at time t; HR(t) = HR at time t.  $\Delta$  = values corrected for resting values. Diff. means = baseline-repeat measurements. All values are adjusted for rate and time of day effects. \* =  $P \leq 0.05$ ; \*\* =  $P \leq 0.01$ ; \*\*\* =  $P \leq 0.0015$ .

<b>Table 4: Reliability of Orthostatic Hypotension and Postural Tachycardia Definitions</b>									
	OH			OH(50)			Sustained Tachycardia		
		Baseline			Baseline			Baseline	
		OH -	OH +		OH(50) -	OH(50) +		PT -	PT +
<b>Repeat</b>	<b>OH -</b>	98	11	<b>OH(50) -</b>	83	12	<b>PT -</b>	110	9
	<b>OH +</b>	11	5	<b>OH(50) +</b>	14	15	<b>PT +</b>	5	1
		<b>κ = 0.21</b>	<b>P=0.009</b>		<b>κ = 0.40</b>	<b>P=0.0000</b>		<b>κ = 0.069</b>	<b>P=0.21</b>

**Table 4:** Reliability of Orthostatic Hypotension (and variants) and Postural Tachycardia definitions. Legend:  $\kappa$  = Cohen's Kappa coefficient. OH = Orthostatic hypotension was defined as sustained failure of SBP or DBP to stabilise to within 20mmHg SBP or 10mmHg DBP of supine levels throughout the active stand from 60 to 110s after standing. OH(50) = impaired blood pressure stabilisation defined as a drop of 20/10mmHg at 50 seconds after standing. Sustained Tachycardia = sustained HR increase of >30bpm or a HR of >120bpm after standing.