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Nanodelivery of Natural Isothiocyanates as a Cancer Therapeutic

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PII: S0891-5849(21)00142-8

DOI: <https://doi.org/10.1016/j.freeradbiomed.2021.02.044>

Reference: FRB 15107

To appear in: *Free Radical Biology and Medicine*

Received Date: 31 August 2020

Revised Date: 31 January 2021

Accepted Date: 26 February 2021

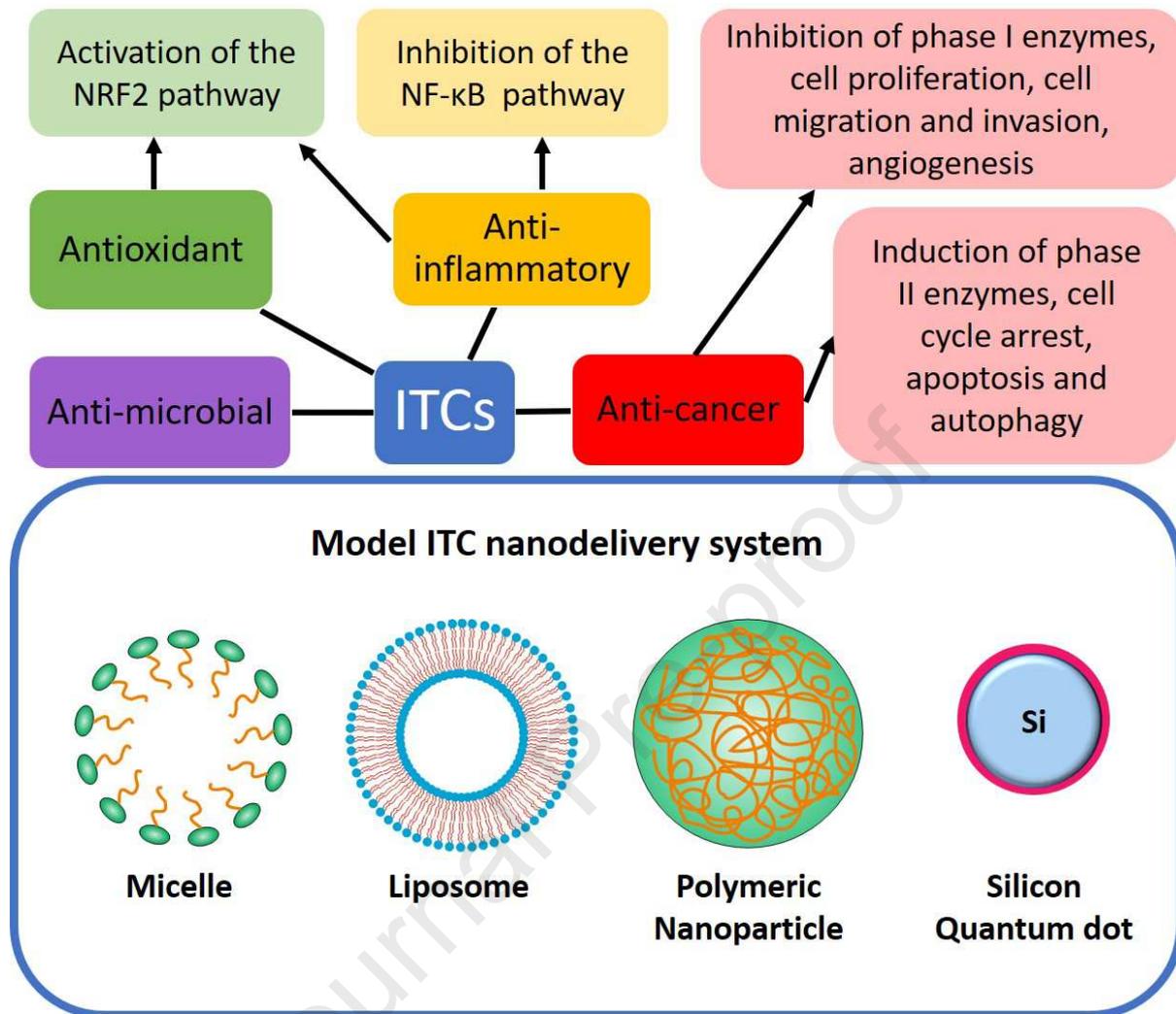
Please cite this article as: Q. Wang, Y. Bao, Nanodelivery of Natural Isothiocyanates as a Cancer Therapeutic, *Free Radical Biology and Medicine*, <https://doi.org/10.1016/j.freeradbiomed.2021.02.044>.

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## Graphical abstract



1 REVIEW ARTICLE

## 2 Nanodelivery of Natural Isothiocyanates as a Cancer Therapeutic

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### 37 **Abstract**

38 Natural isothiocyanates (ITCs) are phytochemicals abundant in cruciferous vegetables with the general  
39 structure,  $R-N=C=S$ . They are bioactive organosulfur compounds derived from the hydrolysis of  
40 glucosinolates by myrosinase. A significant number of isothiocyanates have been isolated from  
41 different plant sources that include broccoli, Brussels sprouts, cabbage, cauliflower, kale, mustard,  
42 wasabi, and watercress. Several ITCs have been demonstrated to possess significant pharmacological  
43 properties including: antioxidant, anti-inflammatory, anti-cancer and antimicrobial activities. Due to  
44 their chemopreventive effects on many types of cancer, ITCs have been regarded as a promising  
45 anti-cancer therapeutic agent without major toxicity concerns. However, their clinical application has  
46 been hindered by several factors including their low aqueous solubility, low bioavailability, instability  
47 as well as their hormetic effect. Moreover, the typical dietary uptake of ITCs consumed for promotion  
48 of good health may be far from their bioactive (or cytotoxic) dose necessary for cancer prevention  
49 and/or treatment. Nanotechnology is one of best options to attain enhanced efficacy and minimize  
50 hormetic effect for ITCs. Nanoformulation of ITCs leads to enhance stability of ITCs in plasma and  
51 emphasize on their chemopreventive effects. This review provides a summary of the potential  
52 bioactivities of ITCs, their mechanisms of action for the prevention and treatment of cancer, as well as  
53 the recent research progress in their nanodelivery strategies to enhance solubility, bioavailability, and  
54 anti-cancer efficacy.

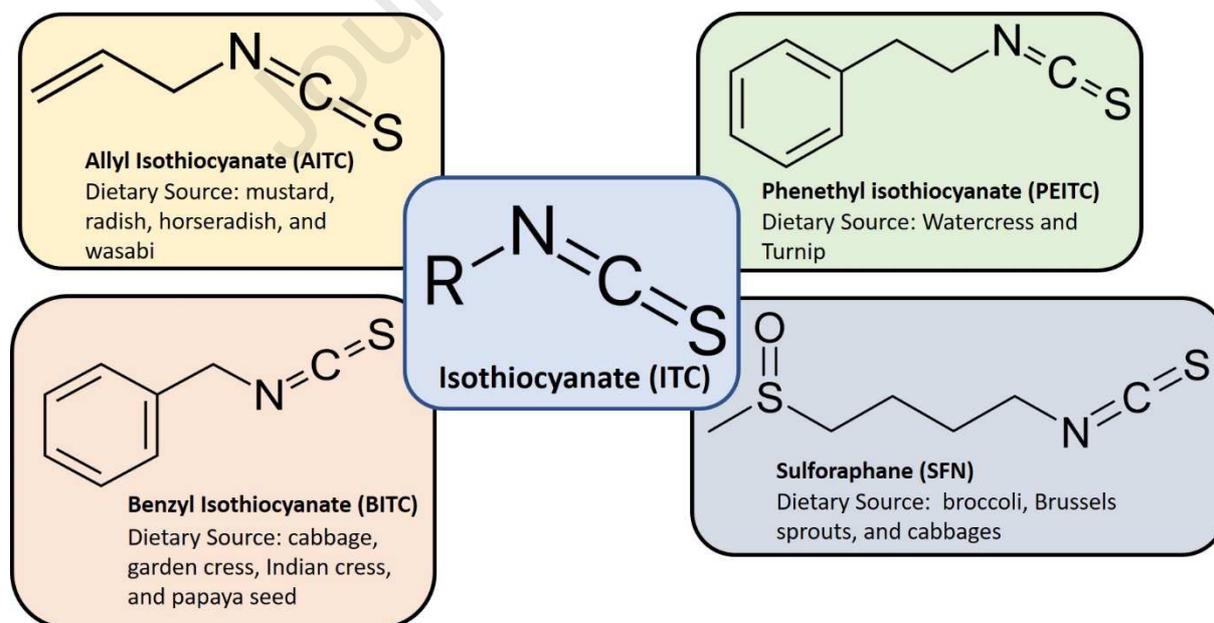
55 **Keywords:** Natural isothiocyanates, Allyl isothiocyanate, Benzyl isothiocyanate, Phenethyl  
56 isothiocyanate, Sulforaphane, Apoptosis, Cancer cells, Cancer therapeutic, Nanoparticle, Nanodelivery  
57 system.

58

## 59 1 Introduction

60 Naturally occurring isothiocyanates (ITCs) are biologically active hydrolysis (breakdown) products of  
 61 glucosinolates from cruciferous vegetables (CVs). ITCs are abundant in a variety of vegetables such as  
 62 broccoli, Brussels sprouts, cabbage, cauliflower, kale, mustard, wasabi, and watercress. They are bioactive  
 63 organosulfur compounds, responsible for the sharp taste of vegetables and active ingredients in their  
 64 defense systems [1]. In CVs, ITCs occur as glucosinolates and are hydrolyzed to ITCs by the action of  
 65 myrosinase enzyme, which is expressed on the external surface of plant cell walls [2]. Additionally, they  
 66 can be released by the action of intestinal microflora present in humans [3]. Each glucosinolate forms a  
 67 different isothiocyanate when its hydrolyzed. For example, sulforaphane (SFN) is derived from the  
 68 hydrolysis of glucoraphanin. SFN was first isolated from broccoli in 1992 [4], and is one of the most  
 69 studied ITCs. Sinigrin, the glucosinolate precursor of allyl isothiocyanate (AITC), is abundant in mustard,  
 70 horseradish and wasabi [5, 6]. The pungent taste of mustard and wasabi is a characteristic of AITC. It is  
 71 also commonly called mustard oil. Garden cress is rich in glucotropaeolin, the precursor of benzyl  
 72 isothiocyanate (BITC), while watercress is a good source of gluconasturtiin, the precursor of phenethyl  
 73 isothiocyanate (PEITC) [7, 8]. The chemical structures of ITCs are summarized in Figure 1. Upon  
 74 ingestion, ITCs are rapidly conjugated to glutathione (GSH) in the gut epithelium or liver [1]. They are then  
 75 metabolized in the mercapturic acid pathway, and sequentially excreted in the urine mainly as  
 76 N-acetylcysteine (NAC) conjugates. In cultured cell and animal models, isothiocyanates have demonstrated  
 77 strong antioxidant and anti-inflammatory activities, as well as potent anti-cancer activities[1, 2, 9, 10]. This  
 78 review summarizes the antioxidant, anti-inflammatory and anti-cancer activities of ITCs with the focus on  
 79 recent progress of ITCs nanodelivery systems in cancer treatment.

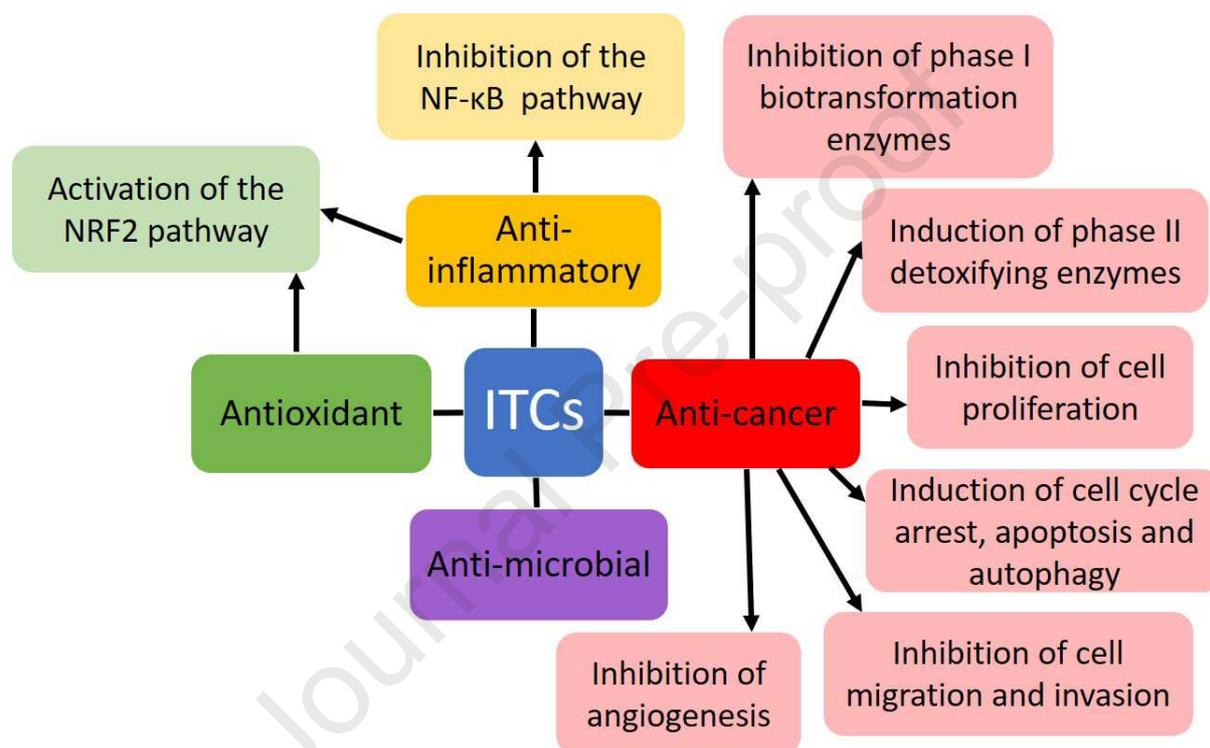
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82 *Figure 1. The basic structure and main types of natural isothiocyanates*

## 83 2 Biological activities of natural isothiocyanates

84 As shown in Figure 1, the chemical structures of ITCs consist of a functional group  $-N=C=S$ , named as  
 85 isothiocyanate group, with various side chains. The central carbon atom of the functional group makes  
 86 ITCs as strong electrophiles. In general, ITCs can react readily with sulfur-, nitrogen- and oxygen-based  
 87 biological nucleophiles, e.g. the thiol and amino groups of proteins [11]. Thus, the biological activities of  
 88 ITCs may be due to the direct reaction with these functional groups in various proteins. The biological  
 89 activities of ITCs and the underlining mechanisms are shown in Figure 2 which will be discussed in the  
 90 following subsections.



91  
 92 **Figure 2. The main biological activities of isothiocyanates**

### 93 2.1 Antioxidant activity

94 Many naturally occurring isothiocyanates, and in particular sulforaphane (SFN), have shown antioxidant  
 95 effects via the activation of the nuclear factor E2-related factor 2 (Nrf2)-dependent pathway [12-14].  
 96 Binding of ITCs to sulfhydryl groups of Kelch-like ECH-associated protein 1 (KEAP1) blocks the cycle of  
 97 KEAP1-dependent Nrf2 degradation, resulting in the release of Nrf2, and is followed by translocation of  
 98 Nrf2 to the nucleus. Nrf2 could then bind to the antioxidant response element (ARE) located in the  
 99 promoters of genes encoding antioxidant/detoxifying enzymes, which includes glutathione S-transferases  
 100 (GSTs), thioredoxin (Trx), NADPH quinone oxidoreductase 1 (NQO-1), and heme oxygenase 1 (HO-1)  
 101 [15]. In a number of animal studies, SFN was shown to have cytoprotective effects on many tissues and  
 102 organs by activation of the Nrf2 pathway [16, 17]. For example, sulforaphane reduced oxidative  
 103 damage-induced vascular endothelial cell injury in a type 2 diabetes mellitus mouse model by upregulation  
 104 of the Nrf2 pathway [17]. Another example includes the attenuation of cellular damage caused by oxidative  
 105 stress in lenses and lens cells by SFN through upregulation of the Nrf2 pathway [18]. Studies have

106 demonstrated that the upregulation of Nrf2/ARE dependent gene expression by ITCs was mediated by the  
107 mitogen-activated protein kinase (MAPK) pathway [19].

## 108 2.2 Anti-inflammatory activity

109 Isothiocyanates, especially sulforaphane exhibited strong anti-inflammatory activity though Nrf2  
110 activation. The anti-inflammatory activities of Nrf2 include transcriptional upregulation of enzymes  
111 encoded by Nrf2-target genes, such as leukotriene B4 dehydrogenase [20], but also the blocking of  
112 pro-inflammatory cytokine transcription, such as IL-6 and IL-1 $\beta$  [21]. In addition, to direct  
113 anti-inflammatory effects mediated through Nrf2 signaling, SFN may impair the redox-sensitive DNA  
114 binding and transactivation of the pro-inflammatory nuclear factor kappa-light-chain-enhancer of activated  
115 B cells (NF- $\kappa$ B) [22], which altogether can lead to a decreased inflammatory response. BITC has greater  
116 affinity to inhibit the NF- $\kappa$ B than SFN due to the presence of additional benzyl structure [23]. The ITC  
117 modulation of Nrf2 and NF- $\kappa$ B pathways are especially important in chemoprevention because both  
118 oxidative stress and inflammation are significant contributors to the progression of cancer.

## 119 2.3 Anti-cancer activity

120 Cancer has been a major research focus over several decades [24]. The increasing understanding of cancer  
121 biology has led to a molecular approach to treat cancer and develop prevention strategies. AITC, BITC,  
122 PEITC, and SFN have been proven to exhibit anti-cancer effects against several different types of cancer  
123 [25-32]. Over the last decade, strong efforts have been made to understand the molecular mechanisms of  
124 ITC anti-cancer activities. SFN is the most studied ICT that acts on several hallmarks of cancer, possesses  
125 chemopreventive and chemotherapeutic potential [33-35]. The hallmarks acquired for tumor evolutions are  
126 genomic instability, sustained proliferative signaling, growth suppressor evasion, resistance to cell death,  
127 replicative immortality, deregulated metabolism, tumor-promoting inflammation, immune system evasion,  
128 angiogenesis and tissue invasion and metastasis [36]. Both *in vitro* and *in vivo* experiments demonstrated  
129 that SFN protects cells from DNA damage, which is mainly mediated by its activity on Phase II detoxifying  
130 enzymes. Phase II enzymes are regulated by the Nrf2-Keap system to maintain the homeostasis of cellular  
131 levels of GSH and Trx, which scavenge reactive oxygen species (ROS) and reactive nitrogen species  
132 (RNS) in cells [37]. The most prominent chemopreventive effect of ITC is associated to its ability to  
133 activate Nrf2 with the subsequent induction of Phase II enzymes. Molecular studies have shown that the  
134 induction on these phase II enzymes from ITCs depends on the ARE and that the regulation is associated  
135 with disruption of Nrf2-KEAP1 interactions and MAPK activation [38]. A lot of studies have proved that  
136 ITCs possess strong abilities to induce the activity of important Phase II enzymes including NQO1, GST,  
137 UDP-glucuronosyltransferase (UGT) and glutamate cysteine ligase (GCL) [4, 10, 27, 39, 40]. However,  
138 recent studies on tumor cell biology demonstrate that Nrf2 activation is not always leads to positive effect  
139 (anti-cancer) in cancer cells, for example aberrant activation of Nrf2 often results from is a common  
140 mutations in non-small cell lung cancer (NSCLC) and is associated with chemoresistance and  
141 radioresistance [41]. Constitutive activation of Nrf2 in cancer cells induces pro-survival genes, promotes  
142 cancer cell proliferation and avoidance of apoptosis, thus increasing cancer therapeutic resistance [37, 42,  
143 43]. The controversial role of the Nrf2-Keap1 pathway in cancer prevention versus cancer progression has  
144 been explained by Kensler and Wakabayashi using a U-shaped dose-response curve [42]. They  
145 hypothesized that the chemopreventive effect only occurs when the expression level of Nrf2 falls within a

146 specific pharmacological range, while outside this range the risk of cancer is increased. In fact, genetic  
147 mutation of Nrf2/Keap1 induces permanent activation of Nrf2 signaling pathway causing cancer  
148 therapeutic resistance. In contrast, the transient activation of Nrf2 due to administration of ITCs has a less  
149 harmful effect [42].

150 There is now sufficient evidence from animal models to show that certain ITCs can also modulate the  
151 activity of phase I biotransformation enzymes, especially those of the cytochrome P450 (CYP) family [2].  
152 In a primary rat hepatocyte-based model, AITC, BITC, PEITC, and SFN have been found to downregulate  
153 CYP3A2 mRNA expression [44]. Also, PEITC could inactivate CYP2E1 through heme destruction and  
154 protein modification [45]. It is suggested that inhibition of specific CYP enzymes involved in carcinogen  
155 activation could prevent the development of cancer.

156 ITCs have also been found to modulate the expression of the cell cycle regulators, cyclins and  
157 cyclin-dependent kinases (CDK), as well as induce apoptosis in a number of cancer cell lines by activating  
158 both extrinsic and intrinsic pathways [46]. AITC was found to induce mitochondrion-mediated apoptosis in  
159 human bladder cancer cells, which depended entirely on mitotic arrest and was mediated via Bcl-2  
160 phosphorylation at Ser-70 [47]. In a mouse model of colorectal cancer, PEITC reduced both the number  
161 and size of polyps, which was associated with the activation of the CDK inhibitor, p21, inhibition of  
162 various cyclins and induction of apoptosis [48]. It has been widely demonstrated that SFN induces caspases  
163 activation, elevating expression of pro-apoptotic Bcl-2 proteins, which induces PARP cleavage and nuclear  
164 chromatin condensation in several cancer cell lines [49-52]. Apoptosis induction by sulforaphane could be  
165 also mediated by the MAPK signaling pathways, e.g. P38 in melanoma cells [51], or ERK and JNK in  
166 prostate cancer cells [53].

167 Several studies have also suggested that ITCs can inhibit cancer cell migration and invasion. For  
168 example, AITC reduced cell adhesion, migration and metalloproteinase (MMP) gene expression in  
169 SK-Hep1 cells [54]. In another study, AITC suppressed the epidermal growth factor (EGF) induced  
170 invasion and migration in HT29 cells [55]. In a breast cancer xenograft mouse model, BITC inhibited high  
171 fat diet-driven promotion of breast tumor growth, as well as lung and liver metastasis [56]. In a mouse  
172 model of breast tumor metastasis, PEITC inhibited the migration of tumor cells to the brain after injection  
173 into the hearts of mice [57]. The anti-migratory effect of SFN was associated with suppression of MMP  
174 [58] and down regulation of epidermal growth factor receptor (EGFR) [59]. SFN inhibited the migration  
175 and invasion of triple-negative SUM159 human breast cancer cells through suppressing the Hedgehog  
176 signaling pathway [60]. The epithelial to mesenchymal transition (EMT) describes a process of epithelial  
177 cell transformation in which the primary tumor cells lose their polarity and adhesion properties while  
178 gaining migratory and invasive properties. It is one of the common properties of tumor invasion and  
179 metastasis [61]. SFN inhibited EMT in thyroid cancer cells is associated with upregulation of E-cadherin  
180 and downregulation of SNAI2, vimentin, MMP-2 and MMP-9 [62]. Angiogenesis is a crucial process in  
181 tumor progression where new capillaries develop from pre-existing blood vessels to support tumor growth.  
182 ITCs have been shown to prevent the formation of such capillary-like structures from human umbilical  
183 endothelial cells, as well as inhibition of the expression and function of hypoxia inducible factors (HIFs)  
184 that control angiogenesis [63].

185 In conclusion, AITC, BITC, PEITC and SFN have efficient chemopreventive and chemotherapeutic  
186 effects. The chemopreventive effects of ITC are associated to its capability to activate the Nrf2-Keap-ARE

187 pathway with the final induction of Phase II enzymes. Nrf2 has a double-edged role in the context of cancer  
188 management. The transient activation of Nrf2 by nutraceutical intervention of ITCs could be beneficial to  
189 healthy people or an at-risk group who is exposed to potential carcinogens. Moreover, the  
190 chemotherapeutic effects of ITC are associated to its ability to modulate cell cycle arrest, induce apoptosis,  
191 and inhibit angiogenesis and tumor metastasis. However, clinical trials are needed to ascertain the possible  
192 beneficial effects of ITCs for adjuvant therapy against cancer, which will be discussed in the following  
193 section.

## 194 3 Natural isothiocyanates in human clinical trials

### 195 3.1 Clinical trials of natural isothiocyanates in cancer

196 A number of Phase I and II clinical trials on natural isothiocyanates are in progress or have been completed  
197 to assess their safety, tolerance, pharmacokinetics, and therapeutic benefit in the context of cancer (Table  
198 1). To date, there are around twenty trials on SFN, four trials on PEITC, and one which is not specified.  
199 These clinical trials are mostly focused on breast cancer and prostate cancer, but also include some other  
200 cancer types including colon, lung, pancreatic, bladder, etc.

201 In a recent intervention study, the total sulforaphane metabolite concentration in urine was 0.08  $\mu\text{M}/\text{mM}$   
202 creatinine in women with abnormal mammograms who consumed  $\sim 81.7$  g/d of cruciferous vegetables [64].  
203 The study has also found that higher cruciferous vegetable intake is associated with decreased cell  
204 proliferation in breast ductal carcinoma in situ (DCIS) tissue, but not in benign or invasive ductal  
205 carcinoma (IDC) tissue. The same group has also examined bioavailability and chemopreventive activity of  
206 supplemental SFN in breast cancer patients [65]. Total sulforaphane metabolites in plasma and urine after  
207 consuming 224 mg glucoraphanin as the SFN source were 0.25  $\mu\text{M}$  and 1.06  $\mu\text{M}/\text{mM}$  creatinine,  
208 respectively. This study suggested that glucoraphanin supplementation is safe to use for a few weeks but  
209 may not be sufficient to produce changes in breast tissue tumor biomarkers (HDAC3/HDAC6, histone H3  
210 lysine 18 acetylation (H3K18ac), Ki-67 and p21). Another Phase II study reports that in patients with  
211 recurrent prostate cancer, administration of 200  $\mu\text{mol}/\text{d}$  of sulforaphane-rich extracts for 20 weeks is safe,  
212 but it does not lead to significant reduction in PSA levels in the majority of patients [66]. In a recent pilot  
213 study, Zhang *et. al.* evaluated the effect of SFN on blood HDAC activity, prostate tissue  
214 immunohistochemistry biomarkers and prostate RNA gene expression in prostate cancer patients using  
215 broccoli sprout extract (BSE) supplementation [67]. Despite urine and plasma SFN metabolites being  
216 statistically higher in the BSE supplementation group, like the breast cancer study there was no significant  
217 difference in HDAC activity or prostate tissue biomarkers. Interestingly, 40 differentially expressed genes  
218 have been identified that correlated with supplemental SFN, including downregulation of two genes  
219 previously implicated in prostate cancer development, *AMACR* and *ARLNC1*. Another pilot study to  
220 investigate the efficacy of a dietary supplement made by broccoli soup on prostate cancer patients  
221 demonstrated some promising results. It has been showed that consuming glucoraphanin-rich broccoli soup  
222 for a year affected gene expression in the prostate and is consistent with a reduction in the risk of cancer  
223 progression. The changes in gene expression and associated oncogenic pathways were attenuated in a  
224 dose-dependent manner.

225 There are only a handful of clinical trials on PEITC to evaluate its potential as an anti-cancer agent and  
226 these are mostly limited to lung cancer. A randomized, placebo-controlled double-blind Phase II clinical  
227 trial, involving volunteers who were cigarette smokers, examined metabolism and excretion of PEITC in  
228 human subjects, as well as the chemopreventive effect of PEITC on tobacco-specific lung carcinogen  
229 4-(methylnitrosamino)-1-(3-pyridyl)-1-butanone (NNK) driven carcinogenesis. After daily administration of  
230 40 mg PEITC, an average of 29% PEITC administered dose was excreted as  
231 N-acetyl-S-(N-2-phenethylthiocarbamoyl)-L-cysteine (PEITC-NAC) in the urine. Overall, the NNK  
232 metabolic activation ratio is reduced by 7.7% with PEITC treatment, which suggested a modest inhibitory  
233 effect of PEITC on NNK induced lung carcinogenicity. In addition, the effects of glutathione S-transferases  
234 M1 and T1 (GSTM1 and GSTT1) genotypes on metabolism and excretion of PEITC and its impact on  
235 NNK metabolism have also been investigated in this study. However, the results were complex and are  
236 poorly understood.

237 In addition, it is worthwhile to mention the studies on commercially available formulations of SFN, such  
238 as Sulforadex® (SFX-01) and BroccoMax®. These formulations, with enhanced SFN bioavailability and  
239 stability, have been evaluated on their own or in combination with other cancer therapeutics, such as  
240 endocrine therapies (ET), aromatase inhibitors (AIs), tamoxifen and fulvestrant. A recent completed Phase  
241 II trial concludes that administration of 300 mg SFX-01 twice a day in combination with ET was safe and  
242 well tolerated in patients with estrogen receptor (ER) positive and Her2 negative metastatic breast cancer  
243 [68]. The combinational therapy showed satisfactory anti-tumor activity and prolonged disease  
244 stabilization.

245 So far, we have seen growing numbers of clinical trials on SFN in forms of dietary supplement as well as  
246 commercial formulations. However equivalent trials on AITC and BITC are still missing. The results of  
247 these clinical trials on SFN only partially confirm its promising anti-cancer potential as demonstrated  
248 during *in vitro* studies, which could be a consequence of its instability, low bioavailability, and the different  
249 effects of SFN in the complex tumor microenvironment. More extensive studies with larger sample sizes  
250 are needed to understand the broad spectrum of applications of ITCs in cancer management. Therefore, it  
251 would be interesting to use nanoparticles to enhance its delivery, which will be discussed in the later  
252 section of this review.

### 253 3.2 Clinical trials of natural isothiocyanates in other diseases

254 A few clinical trials are in the pipeline to evaluate SFN in diseases other than cancer including diabetes  
255 (NCT02801448), kidney disease (NCT04608903), skin disorder (NCT03126539), blood/vascular disease  
256 (NCT01114399, NCT01715480), asthma (NCT01183923) and autism (NCT01474993, NCT02677051,  
257 NCT02879110). Most of these trials are still on going with no results published. Two clinical studies on  
258 type 2 diabetes (T2D) patients showed that intervention with broccoli sprout powder doses (112 or 225  
259  $\mu\text{mol/d}$  of SFN equivalents) for 4 weeks, could reduce serum insulin concentration [69] and achieve  
260 favorable lipid profiles [70]. In a recent Phase II trial, daily consumption of broccoli sprout extract  
261 (containing 150  $\mu\text{mol}$  SFN per dose) effectively reduced fasting blood glucose and glycated hemoglobin  
262 (HbA1c) in obese patients with dysregulated type 2 diabetes [71]. In a Phase II trial on autism spectrum  
263 disorder (ASD), SFN treatment (50-150  $\mu\text{mol/d}$ ) for 18 weeks improved autism-related outcomes in young,  
264 male patients [72]. Findings from these studies would add valuable insight to incorporate SFN into T2D  
265 and ASD treatment methods.

266 Table 1: Summary of human clinical trials on ITCs in cancer therapeutics in progress or completed.

Isothiocyanate	Cancer type	Phase	Status	Information/Result	Reference
SFN	Colon Cancer	Not Applicable	Unknown	To assess cruciferous vegetable intake correlates with histone status and histone deacetylase (HDAC) expression. To measure SFN metabolites in blood as a biomarker.	NCT01344330; clinicaltrials.gov
SFN	Pancreatic Cancer	Not Applicable	Unknown	To determine the feasibility of the application of SFN and quercetin in patients receive palliative chemotherapy.	NCT01879878; clinicaltrials.gov
SFN	Smoking-Related Carcinoma	Early Phase I	Active, not recruiting	To determine 1) whether broccoli sprout/Avmacol® increases the urinary excretion of the mercapturic acid of the tobacco carcinogens. 2) Avmacol® upregulates the NRF2 target gene transcripts. 3) the effects of GSTM1 and GSTT1 genotypes in Avmacol® treatment of detoxification of tobacco carcinogens.	NCT03402230; clinicaltrials.gov
SFN	Head and Neck Cancer	Early Phase I	Active, not recruiting	To determine 1) the bioavailability of SFN in Avmacol®. 2) the level of pharmacodynamic upregulation of NRF2 target gene transcripts that occurs in the oral epithelium of patients.	NCT03182959; clinicaltrials.gov
SFN	Melanoma	Early Phase I	Completed	To determine 1) adverse effects with oral SFN. 2) visual and cellular changes of atypical nevi. 3) SFN levels in the blood (4) effect of SFN on STAT1 and STAT3 expression.	NCT01568996; clinicaltrials.gov
SFN	Lung Cancer	Phase II	Recruiting	To study 1) the effects of SFN to former smokers. 2) whether SFN might reverse some of the lung cell changes associated with future development of lung cancer.	NCT03232138; clinicaltrials.gov
SFN	Breast Cancer	Phase I and II	Recruiting	To determine 1) safety of SFN in doxorubicin (DOX) chemotherapy. 2) if SFN decreases DOX-induced inflammatory responses and enhances Nrf2- and SIRT1-target gene expression. 3) if SFN/DOX treatment mitigates DOX associated cardiotoxicity.	NCT03934905; clinicaltrials.gov
SFN	Breast Cancer	unknown	Completed	To investigate the protective effects of topical SFN on radiation-induced dermatitis.	NCT00894712; clinicaltrials.gov

SFN	Breast Cancer	Phase II	Completed	1) SFX-01(Sulforadex®) 300 mg twice a day was safe and well tolerated in patients with ER positive and Her2 negative metastatic breast cancer. 2) SFX-01 in combination with endocrine therapies (ET) demonstrated anti-tumour activity and prolonged disease stabilisation.	NCT02970682; clinicaltrials.gov [68]
SFN	Breast Cancer	Phase II	Completed	14-day intervention of broccoli sprout (SFN) significantly decreases ki67 positive cells, therefore decreases cellular proliferation.	NCT00982319; clinicaltrials.gov
SFN	Breast Cancer	Phase II	Completed	1) Higher SFN intake is associated with decreased cell proliferation in DCIS 2) No significant decrease in HDAC3, HDAC6, H3K18, Ki-67 and p21 activities between placebo- and SFN-treated interventional groups.	NCT00843167; clinicaltrials.gov [64, 65]
SFN	Prostate Cancer	Not Applicable	Recruiting	To study the oral intake of BroccoMax® (containing SFN) in changes in chemicals that feed prostate cancer.	NCT03665922; clinicaltrials.gov
SFN	Prostate Cancer	Not Applicable	Completed	Consuming glucoraphanin-rich broccoli soup affected gene expression in the prostate of men on active surveillance. Changes in gene expression and associated oncogenic pathways were attenuated in a dose-dependent manner.	NCT01950143; clinicaltrials.gov [73]
SFN	Prostate Cancer	Not Applicable	Completed	To investigate the relationship between ingestion of the bioactive compounds from broccoli and garlic, and prostate metabolism	NCT04046653; clinicaltrials.gov
SFN	Prostate Cancer	Not Applicable	Completed	1) No significant decrease in HDAC3, HDAC6, H3K18, Ki-67 and p21 activity between placebo- and BSE-treated interventional groups 2) 40 differentially expressed genes have been identified that correlated with BSE treatment, including downregulation of two genes previously implicated in prostate cancer development, AMACR and ARLNC1.	NCT01265953; clinicaltrials.gov [67]
SFN	Prostate Cancer	Phase I	Completed	To determine the safety and tolerability of single escalating doses of Sulforadex®	NCT01948362; clinicaltrials.gov
SFN	Prostate Cancer	Phase I	Completed	To determine the safety and tolerability of multiple doses of Sulforadex®	NCT02055716; clinicaltrials.gov
SFN	Prostate Cancer	Phase I and II	Completed	To study the effects of administration a high-sulforaphane broccoli sprout extract on 1) Phase II enzymes expression, 2) lipid and DNA oxidation, 3) serum	NCT00946309; clinicaltrials.gov

SFN	Prostate Cancer	Phase II	Completed	<p>dihydrotestosterone (DHT), testosterone (T) and 3-alpha-diol gluconate(3<math>\alpha</math>-DG) levels.</p> <p>1) 5% of Patients who achieve a 50% decline in prostate-specific antigen (PSA) levels.</p> <p>2) The percentage change in PSA from baseline to the final measured value at the end of study is 35%.</p> <p>3) 90% of patients whose PSA has not doubled.</p> <p>4) The half-life of SFN in blood is 1.8-5.5 hours.</p>	NCT01228084; clinicaltrials.gov [66]
PEITC	Lung Cancer	Phase I	Completed	To determine 1) the maximum tolerated dose of oral PEITC in smokers. 2) pharmacokinetics of PEITC during exposure of 4-(methylnitrosamino)-1-(3-pyridyl)-1-butanone (NNK). 3) the perturbation of NNK metabolism by PEITC.	NCT00005883; clinicaltrials.gov
PEITC	Lung Cancer	Phase II	Completed	To determine 1) the effect of PEITC on urinary levels of NNK metabolism. 2) the effects of GSTM1 and/or GSTT1 Genotype on PEITC-NNK Association and on the metabolism and excretion of PEITC. 3) the effects of PEITC on molecular markers of cell proliferation (Ki-67) and apoptosis (caspase-3 and TUNEL) in bronchial tissue.	NCT00691132; clinicaltrials.gov [74]
PEITC	Oral Cancer	Phase I and II	Completed	To examine the effects of PEITC on oral cells with mutant p53	NCT01790204; clinicaltrials.gov
PEITC	Breast Cancer	Phase III	unknown	To explore the ability of PEITC to improve the restorative effects of radiotherapy in breast cancer patients	NCT02468882; clinicaltrials.gov
ITC	Bladder Cancer	Phase I	Recruiting	To study whether increase of cruciferous vegetable intake with the goal of attaining desirable urinary ITC levels improve bladder cancer survivorship.	NCT04548193 clinicaltrials.gov

267

268

## 269 4 Combinatorial strategies of natural isothiocyanates in cancer therapy

270 The combination of two or more therapeutic agents to specifically target cancer signaling pathways is a  
271 rapidly growing field of cancer therapy [75, 76]. When anti-cancer agents with different effects are  
272 combined, they could achieve greater efficacy with lower doses. This might be an additive or synergistic  
273 effect. A synergistic effect is the effect arising between two or more agents that produce an outcome greater  
274 than the sum of the individual components. Synergistic combination therapy allows each anti-cancer agent  
275 to be used at its optimal dose, with reduced side effects and minimized drug resistance [77]. There is a  
276 growing interest in natural compounds such as natural ITCs, which could be used together with  
277 conventional chemotherapeutic drugs in combination therapy. It has been reported by many studies that the  
278 combinational use of natural ITCs and other anti-cancer agents could achieve synergistic anti-cancer  
279 activity [78-82]. In a recent review, Kamal *et al.* have summarized studies on synergistic combination  
280 therapy of sulforaphane and various anti-cancer agents [83]. For example, SFN significantly enhances the  
281 anti-cancer activity of gemcitabine (GEM) [84], paclitaxel (PTX) and docetaxel (DTX) [85] in breast  
282 cancer, oxaliplatin (OX) in colorectal cancer [86] and cisplatin in prostate and pancreatic cancer [87].

### 283 4.1 Combinational use of ITCs and chemotherapeutic drugs

#### 284 4.1.1 ITCs and cisplatin

285 Cisplatin (cis-diamminedichloroplatinum II, CDDP) is one of the most widely used chemotherapeutic  
286 drugs. However, its clinical application is often limited by low chemosensitivity, systemic side effects [88]  
287 and primary or secondary acquired drug resistance [78, 89]. A combination therapy with CDDP and other  
288 anti-cancer agents that enhance tumor sensitivity and decrease unwanted systemic toxicity would present a  
289 significant therapeutic benefit. Di Pasqua *et al.* have studied the combination of natural ITCs and CDDP on  
290 non-small cell lung cancer [90]. BITC and PEITC, but not SFN, are sensitize human non-small cell lung  
291 cancer NCI-H596 cells to various concentrations of cisplatin. The effect is synergistic rather than additive.  
292 They have found that neither cellular platinum accumulation nor DNA-platination account for the enhanced  
293 cytotoxicity, suggested the depletion of  $\beta$ -tubulin with pre-treatment of BITC or PEITC might be important  
294 for sensitization.

295 Wang *et al.* have examined the combination therapy of PEITC and cisplatin in cervical and breast cancer  
296 cells [91]. Treatment of 5  $\mu$ M PEITC with 10  $\mu$ M CDDP exhibits a synergistic effect on the induction of  
297 apoptosis in HeLa cells. The same effect has also been showed in MCF7 breast cancer cells, but not in  
298 normal MCF-10A cells, suggesting the normal MCF-10A cells are more resistant to the cytotoxic effects of  
299 PEITC plus CDDP than MCF-7 breast cancer cells. The selective toxicity of PEITC and CDDP  
300 combination therapy towards breast cancer cells could be a promising safer strategy for breast cancer  
301 treatment. Such synergistic effect was specifically blocked by a MEK1/2 inhibitor, but not by JNK or p38  
302 inhibitors, signifying that ERK activation is involved in the mechanism of synergism. Interestingly, the  
303 researchers found that NF- $\kappa$ B signaling pathway is not involved in the synergistic effects of PEITC and  
304 CDDP.

305 Ling *et al.* reported that the combination of AITC with CDDP synergistically inhibits cancer cell growth  
306 and induces cell death *in vitro* and *in vivo* [79]. Their study revealed that AITC and CDDP combination

307 significantly inhibits cell growth and colony formation in comparison to single agent treatment in both  
308 OV-2008 ovarian cancer cells and HOP62 lung cancer cells. The combination therapy also enhances  
309 apoptosis in association with the downregulation of anti-apoptotic proteins Bcl-2 and surviving. The  
310 combination index (CI) was then calculated using Chou-Talalay equation to verify the type of interaction  
311 between AITC and CDDP in A549 and Hop62 lung cancer cells. A high synergistic effect ( $CI < 0.5$ ) has  
312 been found for the combinational treatment of AITC at 10-20  $\mu\text{M}$  and CDDP at 8-16  $\mu\text{M}$ . Further *in vivo*  
313 study on human lung cancer xenografts demonstrated that combination of AITC with CDDP could  
314 significantly suppress tumor growth without an observable increase in systemic toxicity in comparison with  
315 single agent treatment. Furthermore, their data revealed that addition of AITC to CDDP changes the profile  
316 of G2/M phase arrest and significantly extends the duration of G2/M phase arrest in comparison with single  
317 treatment. Like BITC and PEITC [88], the synergistic effects of AITC with CDDP have been found to be  
318 associated with rapid  $\beta$ -tubulin depletion and microtubule dysfunction.

319 In SFN and CDDP combination therapy against pancreatic and prostate cancer, MIA-PaCa2 and DU145  
320 cells were exposed to treatment for 72 h and analyzed by MTT assay and morphological evaluation [87]. It  
321 was found that SFN increased the *in vitro* cytotoxicity from CDDP in both cell lines. SFN and CDDP  
322 combined treatment also showed significantly enhanced apoptosis compared to single agent alone. Another  
323 study done by Kerr *et al.* reported the enhancement of anti-cancer activity of CDDP when combined with  
324 SFN against squamous cell carcinoma cells SCC-13 and HaCaT [92]. An increased suppression of cell  
325 proliferation, stem cell spheroid formation, and cell migration was observed in combination treatment  
326 compared to each agent alone. It is worth noting that several studies performed on combination therapy of  
327 SFN and CDDP suggested their synergistic effect might be caused by several mechanisms. Kaminski *et al.*  
328 reported combined treatment of SFN and CDDP in human ovarian carcinoma A2780 and SKOV3 cell lines  
329 results in synergy and antagonism, respectively. While SFN significantly potentiated CDDP-induced DNA  
330 damage in A2780 cells, it protected SKOV3 cells against CDDP-crosslinking. Such dual effects of SFN  
331 may be explained by different activation of the Nrf2 pathway [78]. A later study reveals that SFN and  
332 CDDP combination therapy induced a synergistic anti-cancer effect on malignant mesothelioma (MM)  
333 cells by enhancing ROS stress and mitochondrial membrane depolarization [93].

#### 334 4.1.2 ITCs and taxanes

335 Nunez-Iglesias *et al.* investigated the cytotoxic effects of glucosinolate-degradation products (AITC,  
336 PEITC, SFN, 4-pentenyl-isothiocyanate (4PI), iberin (IB), or indole-3-carbinol (I3C)) in absence or  
337 presence of DTX in androgen-independent human prostate cancer PC3 and DU145 cells. It was observed  
338 that the combination therapy of ITCs and DTX was more effective in reducing viability of prostate cancer  
339 cells compared with each agent alone. The index of survival rate has been used to calculate the interaction  
340 of ITCs and DTX. It was found that the combination of DTX with AITC or PEITC significantly caused a  
341 synergistic sensitization of PC3 and DU145 for DTX induced apoptosis and DTX induced cell growth  
342 inhibition [94]. They have also suggested potential mechanism for the synergistic effect, such as  
343 degradation and polymerization of  $\alpha$  and  $\beta$  tubulin, modulation of the intracrine metabolism of androgens  
344 mediated by CYP3A4, and the expression of efflux transporters and/or GSH activity. Burnett *et al.* studied  
345 the combination effect of sulforaphane with paclitaxel or docetaxel on SUM149 and SUM159 breast cancer  
346 cells *in vitro* and *in vivo* [85]. *In vitro* results suggested that combination of a minimally cytotoxic SFN  
347 treatment (5  $\mu\text{M}$ ) with either PTX or DTX lowered their IC50s to less than 50% of the original value. *In*

348 *in vivo* study with SUM149 implanted NOD/SCID mice also showed similar effects when treated with SFN  
349 and DTX combination.

350 Overall, natural ITCs are proven to potentiate the activity of several classes of chemotherapeutics  
351 including cisplatin, paclitaxel, and docetaxel through additive and synergistic effects. Such combinational  
352 therapy has efficacy against a variety of cancer types in several model systems. Further clinical studies are  
353 needed to evaluate safety and efficacy of the combinational use of ITCs with chemotherapies.

## 354 4.2 Combinational use of ITCs and other anti-cancer agents

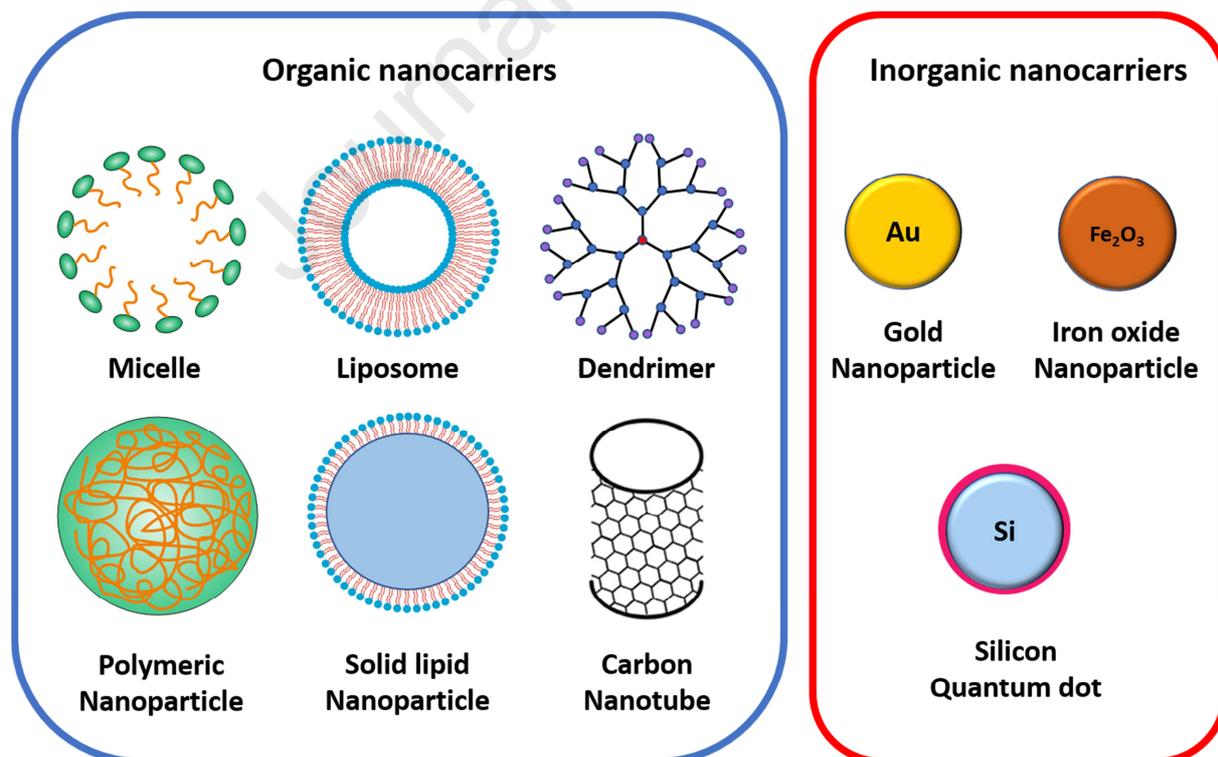
355 Gupta *et al.* reported synergistic anti-cancer activity of laccaic acid (LA) and PEITC combination in  
356 colorectal cancer via dual inhibition of DNA methyltransferase-1 and Histone deacetylase-1. In the HT29  
357 cell line, treatment with the combination showed reduced cell viability with increased apoptotic cell death  
358 compared to LA and PEITC alone. In the *in vivo* study using a 1,2-dimethyl hydrazine induced colon  
359 cancer rat model, combination therapy significantly improved mortality, fecal consistency score, IL-6,  
360 TNF- $\alpha$ , DNMT1 and HDAC1 levels, and attenuated the number of aberrant crypt foci which depicted a  
361 better prognosis [80].

362 A recent study combined a classical antihistaminic drug, Loratadine (LOR) and SFN using a  
363 self-microemulsifying drug delivery system. Combination of a minimally cytotoxic SFN treatment with  
364 LOR achieved a 95% reduction of the LOR IC<sub>50</sub> value in MIA PaCa-2 cells and a 90% reduction in Panc-1  
365 cells [95], which suggested SFN largely enhanced the anti-cancer activity of LOR in pancreatic cancer.  
366 Another study found that combinational use of salinomycin (SAL) and SFN synergistically inhibited cell  
367 viability, proliferation, migration and invasion and enhanced apoptosis in Caco-2 and CX-1 cells. Similar  
368 results were also seen in the xenograft model. In the combination therapy, decreased expression of PI3K,  
369 p-Akt and Bcl-2 and increased expression of Bax, p53 and cleaved PARP suggests PI3K/Akt pathway is  
370 involved in synergistic effect of SAL and SFN induced apoptosis [96]. Synergistic effects of SFN were also  
371 observed in triple combination therapy. A combination of curcumin (CUR), SFN, and dihydrocaffeic acid  
372 (DHA) was evaluated against human colon cancer cells [97]. At cytotoxic concentrations designed to kill  
373 50% and 75% of cells, the effects of CUR-DHA, SFN-DHA, and CUR-SFN-DHA combination were  
374 additive, while SFN-CUR combination showed a relatively high antagonistic effect. Interestingly, at 90%  
375 cytotoxicity, SFN-DHA combination exerted a significant synergistic effect. This combination is  
376 significantly more cytotoxic for cancer cells than healthy cells. These studies on combination strategies of  
377 ITCs provided ample evidence that combining ITCs with other anti-cancer agents pose a potential way  
378 forward for improved outcome. Further nanoformulation based on these combination therapies could result  
379 in additional enhancement of anti-cancer efficacy through targeted delivery.

## 380 5 Nanodelivery of natural isothiocyanates in cancer therapy.

381 The bioactivity of ITCs is largely dependent on the absorption, metabolism, distribution, and excretion in  
382 human body. Despite various cellular and animal models confirming the benefit derived from many ITCs  
383 against cancer, the clinical utilization of ITCs is still limited [98-100] due to its low solubility, stability, and  
384 bioavailability, as well as the “biphasic dose response”. To overcome these drawbacks, scientists have  
385 employed recently developed nanodelivery technology. In these applications, nanomaterial has been  
386 employed as transport modules to carry ITC and/or other chemotherapy agents to achieve therapeutic

387 synergism in cancer treatment. Different types of nanodelivery systems have been developed for this  
 388 purpose. These nanodelivery systems can be easily fabricated to selectively target tumor cells as opposed to  
 389 normal cells [101]. Some of the main nanodelivery systems used in cancer therapeutics are micelles,  
 390 liposomes, dendrimers, polymeric nanoparticles, carbon nanotubes, quantum dots (QDs), magnetic iron  
 391 oxide nanoparticles and gold nanoparticles. Figure 3 shows a schematic representation of major  
 392 nanodelivery systems used in cancer therapy. A micelle is a self-assembly vesicle with an outer hydrophilic  
 393 tail region and hydrophobic core center [102]. A nanosized liposome represents a self-assembled  
 394 phospholipid bilayers vesicles entrapping one or more aquatic compartments [103, 104]. A dendrimer is a  
 395 highly branched, symmetric, star-shaped macromolecule with nanometer-scale dimensions [105]. A  
 396 polymeric nanoparticle can be synthesized using biodegradable and biocompatible polymers or copolymers  
 397 [106]. A solid lipid nanoparticle (SLP) contains a surfactant outer layer and lipids in solid phase with the  
 398 advantage of entrapping lipophilic molecules without applying organic solvents [107]. Both gold and iron  
 399 oxide nanoparticles are metallic nanoparticles which have imaging functionalities used for either passive or  
 400 active drug delivery in cancer diagnosis and treatment. QDs are semiconductor crystals in the range of 2–10  
 401 nm, which possess strong photoluminescence [108-111]. Most importantly, these inorganic nanoparticles  
 402 can be synthesized and modified with various chemical functional groups which facilitate their application  
 403 as drug carriers for cancer therapeutic agents [111, 112]. Anti-cancer therapeutic agents e.g., ITCs can be  
 404 encapsulated within the NP carriers or be physically adsorbed on or chemically linked to the NP surfaces.  
 405 Many nanodelivery systems loaded with ITCs have been proven to be efficacious in inhibiting cancer cell  
 406 proliferation, migration, and invasion. Results from studies reporting anti-cancer effects of the ITC  
 407 nanodelivery systems are discussed in subsections below.



408

409 *Figure 3. Schematic representation of major nanodelivery systems for cancer treatment*

410

## 411 5.1 Nanodelivery of AITC

412 The obstacles to the direct clinical application of AITC include poor aqueous solubility, instability at high  
413 temperature, and susceptibility to degradation by nucleophilic molecules such as H<sub>2</sub>O or those containing  
414 -OH, -SH and -NH<sub>2</sub> groups [113, 114]. AITC is easily hydrolyzed to allylamine in aqueous solution and  
415 was reported to decompose by up to 75% when incubated in water at 37°C for 10 days [115]. Several  
416 encapsulation methods using nanodelivery systems have been employed to protect AITC against  
417 degradation and enhance targeted delivery to cancer cells.

418 Li *et al.* prepared an oil-in-water AITC nanoemulsion by the emulsion inversion point (EIP) method  
419 [116]. They studied the optimal hydrophilic–lipophilic balance (HLB<sub>op</sub>) value of surfactants containing  
420 Tween 80 and Span 80 and synthesized nanodroplets with diameters of 137–215 nm. Over a 6.5 month  
421 period, the nanodroplet sizes and the counts (polydispersity indication) decreased only slightly by 4–13%  
422 indicating the nanoemulsion was very stable in aqueous storage conditions. Moreover, the nanoemulsion  
423 demonstrated superior protection against AITC degradation (78% remaining after 60 days at 30°C), as  
424 compared with zein protein nanoparticles (undetectable after 60 days storage) as well as non-encapsulated  
425 aqueous dispersion (4% remaining after 60 days at 30°C). Their work suggests that nanoemulsion is a  
426 promising approach to enhance the aqueous stability of AITC and may also be applicable to the  
427 stabilization of other chemicals that are susceptible to nucleophilic degradation in aqueous systems.

428 In the studies of Encinas-Basurto *et al.*, AITC has been encapsulated into poly (lactic-glycolic acid)  
429 nanoparticles (PLGA NPs) to extend its shelf life and enhance its antiproliferative properties [117]. The  
430 AITC-loaded PLGA NPs were synthesized using a simple emulsion-solvent evaporation method. The  
431 obtained AITC PLGA NPs had a particle size of  $200 \pm 3$  nm with a polydispersity  $> 2\%$ , and  
432 zeta-potentials of  $-8.0 \pm 0.9$  mV. These nanoparticles demonstrated reduced degradation, volatility and an  
433 extended shelf life when compared with free AITC. *In vitro* cell viability and uptake of AITC PLGA NPs  
434 in cancerous HeLa and MDAMB-231 cells showed that the sustained release of AITC from polymeric NPs  
435 resulted in a significant toxicity towards tumor cells. Thus, PLGA NPs could be used as protective  
436 nanodelivery systems to enhance the biological activity of AITCs. The same group subsequently modified  
437 the surface of AITC PLGA NPs further using a specific antibody to target the Epidermal Growth Factor  
438 (EGF) receptor overexpressed on the epithelial squamous carcinoma cells [118]. AITC-loaded PLGA NPs  
439 showed more effective anti-cancer properties when compared with free AITC. The attachment of the  
440 anti-EGFR antibody on the NP's surface further enhanced their cytotoxicity towards the tumor cells. This  
441 targeting ability was additionally tested by co-culturing cervical HeLa cells (EGFR low) and A431 cells  
442 (EGFR overexpressed). The antibody bonded NPs were solely localized in A431 cells, whereas  
443 non-functionalized (no antibody bonding) NPs were distributed randomly between both cell types and at  
444 much lesser extents. These findings demonstrated a successful nanodelivery strategy that not only enhances  
445 the delivery of natural anti-cancer compounds to the tumor tissue, but also specifically targets the tumor  
446 cell receptors followed by tumor sensitization.

447 Liu *et al.* took a different approach to make AITC-conjugated silicon quantum dots (AITC-SiQDs) for  
448 the treatment of liver cancer [119]. To prepare the AITC-SiQDs, hydrogen terminated SiQDs were  
449 synthesized by galvanostatic anodization of a porous silicon layer [120], followed by a reaction with allyl  
450 bromide. The bromine-functionalized QDs were further reacted with potassium thiocyanate to form  
451 isothiocyanate-functionalized SiQDs, i.e., AITC-SiQDs. The obtained AITC-SiQDs were sphere shaped

452 and around 4 nm in diameter. The AITC-SiQD size is much smaller than other AITC polymeric NPs but  
453 was in agreement with the SiQD size in previous study [120]. The resultant QDs showed similar  
454 anti-cancer properties compared to free AITC at high doses while avoiding the low doses stimulation  
455 effect. After one hour of incubation with AITC-SiQDs, the intrinsic fluorescence of SiQDs was detectible  
456 inside HepG2 cells. The fluorescent signal optimum at around 12 hours indicating the internalization of a  
457 large number of AITC-SiQDs. In addition, AITC-SiQDs exhibited a lower but long-lasting activation of  
458 Nrf2 which correlated with their levels of cellular uptake. These findings suggested the SiQD nanodelivery  
459 system could be a promising platform to avoid the biphasic effect of free AITC, and that AITC-SiQDs have  
460 the potential to be used in anti-cancer treatment.

461 One of the notable works performed by Chang *et al.* was synthesized the water-soluble AITC NPs using  
462 oil-in-water (O/W) microemulsion [121]. The obtained AITC NPs were about 9.4 nm and stable during  
463 heating up to 110 °C or under three freeze-thawing cycles in DMEM. AITC NPs effectively inhibited  
464 proliferation and migration of HT1376 cells, which showed improved anti-cancer and antioxidant activities  
465 when compared to free AITC. Moreover, compared to AITC alone and empty NPs, these AITC NPs  
466 possessed a better inhibitory effect on lipopolysaccharide (LPS)-induced TNF- $\alpha$ , IL-6, nitric oxide (NO)  
467 and inducible nitric oxide synthase (iNOS) production in RAW 264.7 macrophage cells. These results  
468 demonstrated the potential of AITC nanoemulsion as a therapeutic agent for the treatment of bladder  
469 cancer.

470 Both nano and micro emulsions have been used to improve solubility and stability of AITC in biological  
471 systems. The obtained AITC nanoparticles demonstrated improved anti-cancer and antioxidant activities  
472 when compared to free AITC. The attachment of targeting motifs to the nanoparticle surface could further  
473 enhance their efficacy towards tumor cells.

## 474 5.2 Nanodelivery of BITC

475 In recent years, BITC has been of special interest due to its distinct *in vitro* and *in vivo* anti-cancer abilities,  
476 and antiproliferative and antimicrobial properties [122-124]. Like AITC, due to its strong electrophilic  
477 nature, BITC can easily reacts with nucleophiles under physiological conditions. It also has a characteristic  
478 pungent smell, poor solubility, limited bioavailability and is strongly volatile. Such properties impede its  
479 potential as an effective anti-cancer agent while the research community is still struggling to find an  
480 appropriate delivery system to overcome all its shortcomings. Nanoencapsulation methodology could  
481 potentially increase BITC absorption, stability, activity, and decrease its excretion from the circulatory  
482 system. Furthermore, such nanodelivery systems may have the ability to enhance BITC therapeutic  
483 performance and reduce toxicity, ease of handling and improve its shelf live.

484 Qhattal *et al.* reported an oil-in-water nanoemulsion system to entrap BITC [125]. The nanoemulsion  
485 was prepared by either spontaneous self-nanoemulsification or homogenization-sonication. Both the  
486 nanoemulsion achieved high encapsulation efficiency (EE) of BITC with low polydispersity and good  
487 colloidal stability. In addition, the BITC nanoemulsion showed enhanced aqueous solubility as compared to  
488 pure BITC. They were also easily taken up by human cancer cells A549 and SKOV-3 and inhibited cancer  
489 cell growth. Later, Kumar *et al.* encapsulated BITC in a nanoemulsion through ultrasonication using Tween  
490 80 or decyl- $\beta$ -d-glucopyranoside as stabilizer [126]. The average size of nanoemulsion particles were found  
491 to be  $31.68 \pm 1.78$  nm and a near complete EE value of 99%. The nanodelivery system showed good

492 stability at pH 5, 7 and 9. Under highly acidic or basic conditions, i.e., at pH 2 and 12, the size of NP  
493 increased abruptly as the storage time increased. The occurrence of aggregation might be due to ineffective  
494 electrostatic repulsion and hydrolysis [127, 128]. The BITC nanoemulsion showed improved anti-cancer  
495 activity against breast cancer cell lines as compared to its bare administration.

496 In a recent research, Uppal *et al.* developed cerium oxide nanoparticles (Cerium) based drug delivery  
497 system using ultrasonic nanoemulsification [129]. The synthesized NPs (size  $\leq 5$  nm) were then loaded with  
498 BITC. The average particle size of BITC Cerium NPs were  $5.1 \pm 0.8$  nm with zeta-potential value of  $-14.92$   
499  $\pm 1.1$  mV. The formulation achieved high encapsulation efficiency and a good drug loading. Compared to  
500 Cerium alone, these NPs inhibited cell viability more effectively in MDA-MB 231 cells. The same group has  
501 also produced a new rhamnolipid based nanoemulsion system employing the heating stirring-sonication  
502 method [130]. The optimized nanoemulsion exhibited good long-term stability, very high encapsulation  
503 efficiency, sustained release and increased cytotoxicity against MDA-MB 231 cells as compared to BITC  
504 alone.

505 Overall, nanoemulsification is the main synthesis method used for entrapping BITC toin nanodelivery  
506 systems. These BITC nanoemulsionsnanoemulsion show enhanced absorption and bioavailability as well  
507 prolonged shelf-life. High encapsulation efficiency along with a sustained release can be achieved by  
508 nanoemulsionsnanoemulsion. Finally, compared to its free form, BITC nanoemulsion showed improved  
509 anti-cancer activity against several cancer cell lines.

### 510 5.3 Nanodelivery of PEITC

511 PEITC, a naturally occurring isothiocyanate, has been reported to have good anti-cancer activity in both *in*  
512 *vitro* and *in vivo* models [74, 131, 132]. Several studies have reported that PEITC could inhibit proliferation  
513 and induce apoptotic cell death in several cancer cell lines, including breast cancer [31], prostate cancer  
514 [133], cervical cancer [134], lung cancer [74] and liver cancer [30, 135, 136]. Several studies have also  
515 suggested that PEITC can sensitize cancer cells to chemotherapy drugs such as cisplatin and doxorubicin  
516 (DOX), demonstrating a synergistic effect. Nanotechnology has allowed the development of new  
517 nanodelivery systems that can be used to explore such potential in cancer treatment.

518 Pasqua *et al.* showed that PEITC could enhance the efficacy of CDDP in non-small cell lung cancer [90].  
519 Based on this concept, liposomal nanoparticles containing both PEITC and CDDP have been developed  
520 [137]. The resultant NPs were approximately 130 nm, with a high negative zeta-potential of  $-65$  mV. The  
521 drug loading of CDDP and PEITC were approximately 1% w/w each. In NCI-H596 NSCLC cells,  
522 liposomes containing a combination of CDDP and PEITC showed the greatest toxicities among all  
523 treatments. These liposome NPs are also highly stable in circulation. The protective formulation allows  
524 synergistic treatment of CDDP and PEITC to reduce the NSCLC tumor more effectively with fewer side  
525 effects than free CDDP and PEITC treatments. Thus, they could be a promising system for clinical  
526 development. Sun *et al.* has further expanded their work to use a lesser amount of CDDP than the previous  
527 formulation (1:3 ratio of CDDP to PEITC compared to 1:2 ratio of CDDP to PEITC) [138]. The optimized  
528 nanoliposome formulation was much more toxic towards both A549 and H596 human NSCLC cell lines  
529 than the WI-38 and BEAS-2B human normal lung cell lines. These findings suggest that combined PEITC  
530 and CDDP nanoliposomes have good specificity and selectivity toward tumor tissues and could provide a  
531 promising cancer treatment.

532 Pulliero *et al.* evaluated the ability of nanoliposomes to modify the pharmacodynamics of PEITC [139].  
533 The nanoliposomes with a mean size of 70 nm were synthesized using  
534 (1,2-di-O-octadecenyl-3-trimethylammonium propane (DOTMA), cholesterol and D-alpha-tocopheryl  
535 polyethylene glycol succinate (TPGS) by a simple ethanol injection method. Their data suggested that  
536 PEITC NPs significantly increased the ability of PEITC to protect against cigarette smoke condensate  
537 induced DNA damage and enhanced its ability to activate protective apoptosis in bronchial epithelial cells  
538 both *in vitro* and *ex vivo*.

539 Seema *et al.* designed a PEITC nanocomposite using graphene oxide (GO) as nanocarrier [140]. GO has  
540 a unique graphene basal plane that could be modified with functional groups such as carboxylic (COOH),  
541 hydroxyl (OH) and epoxides groups etc. These functional groups enable further functionalization of GO  
542 with drug loading and biomolecules (e.g., RNA/DNA). The nanocomposite was around 6 nm and exhibited  
543 sustained release of PEITC under both physiological and intracellular lysosomal conditions. Cell viability  
544 assays suggested that the nanocomposite has much better anti-cancer activity against HepG2 liver cancer  
545 cells when compared to the crude PEITC and was also found to be nontoxic to normal 3T3 cells. This study  
546 demonstrated that PEITC conjugated GO could be an efficient nanodelivery system for pharmaceutical  
547 applications in cancer therapies.

548 In a recent study, Wu *et al.* established a complex black phosphorus nanosheets (BPN) based  
549 nanodelivery system for simultaneously delivery of DOX and PEITC. The BPNs/DOX was first coated  
550 with a polydopamine (PDA) layer through dopamine polymerization, followed by binding of polyethylene  
551 glycol-amine (PEG-NH<sub>2</sub>) via the Schiff base reaction [141]. The BPNs-PDA-PEG/DOX was then  
552 conjugated with PEITC and this system was shown to effectively decrease mutant p53 levels in resistant  
553 cancer cells and enhance DOX sensitivity. Furthermore, the phenolic hydroxyl groups of  
554 BPNs-PDAPEG-PEITC/DOX can chelate manganese ions (Mn<sup>2+</sup>) which exhibit a strong T1 contrast in  
555 magnetic resonance imaging (MRI). Thus, BPNs-PDA-PEG-PEITC-Mn/DOX could be used as  
556 theragnostic agent for MRI-guided photothermal therapy/photodynamic therapy (PTT/PDT) as well as  
557 synergistic chemotherapy to overcome drug-resistance. Both *in vitro* and *in vivo* experiments have  
558 demonstrated the BPNs-based drug delivery system has effectively inhibited drug resistance tumor with  
559 minimal side effects. This triple synergistic nanodelivery system has a great application potential in the  
560 treatment of MDR breast cancer.

561 Several distinct nanodelivery systems have been developed for PEITC including nanoliposomes,  
562 nanocomposite using graphene oxide and black phosphorus nanosheets. Nanodelivery of the combinational  
563 therapies of PEITC with cisplatin or doxorubicin exhibit enhanced anti-cancer efficacy with reduced side  
564 effects. These synergistic nanodelivery systems have good specificity and selectivity towardstoward tumor  
565 tissues and could provide a promising application potential in the treatment of non-small cell lung cancer  
566 and breast cancer.

## 567 5.4 Nanodelivery of SFN

568 Sulforaphane is one of the most studied natural ITCs and has significant antioxidant, anti-inflammatory and  
569 anti-cancer activities. *In vitro* and *in vivo* studies have confirmed the chemoprotective effects of SFN in  
570 various tumors, including those of the breast, prostate, lung, and colon through variety of molecular  
571 mechanisms [33, 142-144]. Moreover, a number of studies have suggested that SFN may target cancer stem

572 cells (CSCs) in different types of cancer through activation of microRNA-124 (miR-124), modulation of  
573 NF- $\kappa$ B, sonic hedgehog (SHH), epithelial-mesenchymal transition and Wnt/ $\beta$ -catenin pathways [145-147].  
574 However, due to high lipophilicity, poor aqueous solubility, and low stability due to sensitivity to oxygen,  
575 heat and alkaline conditions, the therapeutic potential of SFN is greatly hindered. To enhance its aqueous  
576 solubility and bioavailability, several different nano formulations of SFN have been developed, including  
577 polymeric nanoparticles, micelles, liposome, carbon dots, metallic and magnetic nanoparticles. In addition,  
578 using an advanced nanodelivery system, SFN can be combined with other phytochemicals and  
579 chemotherapies to achieve synergistic effects towards tumor cells, e.g., CUR, DTX and CDDP.

580 Huang *et al* designed a combined docetaxel and sulforaphane loaded poly (D,  
581 L-lactide-coglycolide)/hyaluronic acid (PLGA-b-HA) based nanoparticle [148] to simultaneously target  
582 differentiated breast cancer cells (DBCCs) and breast cancer stem cells (BCSCs). Both *in vitro* and *in vivo*  
583 analyses showed the DTX and SFN combined NPs have enhanced cytotoxicity toward both DBCCs and  
584 BCSCs compared with the free drugs. In addition, the self-renewal ability of BCSCs was strongly inhibited  
585 by the SFN-loaded NPs *in vivo*, and the inhibition of BCSCs *in vitro* was probably caused by  
586 down-regulating beta-catenin expression. The combination of SFN and DTX loaded NPs demonstrates their  
587 great therapeutic potential in the treatment of breast cancer.

588 Manjili *et al* fabricated novel SFN encapsulated gold-coated iron oxide nanoparticles [149]. The surface  
589 of gold-coated iron oxide NPs was functionalized with thiolate polyethylene glycol-folic acid and thiolate  
590 polyethylene glycol-FITC for SFN loading. The average diameter of the synthesized NPs was  
591 approximately 38 nm. The SFN loaded NPs were more cytotoxic than the no-loading NPs in MCF-7 cells  
592 as proved by cell viability and apoptosis assay. In addition, the expression rates of the anti-apoptotic genes  
593 (bcl-2 and bcl-xL) in MCF-7 cells were significantly decreased by exposure to SFN NPs. Overall, this  
594 study has exhibited a novel design of gold-coated iron oxide NPs, which could be developed as a potential  
595 nanodelivery system to improve the efficiency and stability of SFN as an anti-cancer therapy.

596 Danafar *et al.*, have established a micellar nanodelivery system using monomethoxypoly (ethylene  
597 glycol)-poly (varepsilon-caprolactone) (mPEG-PCL) [150]. SFN was encapsulated within mPEG-PCL  
598 micelles through a single-step nano-precipitation method. The obtained micelles have spherical shapes with  
599 size of 107 nm. The encapsulation efficiency of SFN was  $86 \pm 1.58\%$  and they also achieved a remarkable  
600 level of sustained release *in vitro*. The SFN loaded nanomicelles significantly inhibited viability and  
601 induced apoptosis in MCF-7 cells, which suggests that SFN loaded nanomicelles could be an effective  
602 breast cancer treatment strategy in the clinic. The same group have developed another micellar NP using a  
603 tri-block copolymer poly (caprolactone)-poly (ethylene glycol)-poly (caprolactone) (PCL-PEG-PCL)  
604 [151]. Micelle characterization and stability, the particle size and their morphology were determined by  
605 DLS and AFM. The loading efficiency of SF was  $19.33 \pm 1.28\%$ . The resultant micelles were the same size  
606 as the mPEG-PCL micelles. The results of *in vivo* experiments indicated the SFN loaded micelles prolong  
607 the circulation period and increase the therapeutic efficacy of SFN. Later, this group has developed a  
608 combined anti-cancer nanodelivery strategy using curcumin (CUR), sulforaphane and PEGylated gold  
609 coated Fe<sub>3</sub>O<sub>4</sub> magnetic nanoparticles (PEGylated Fe<sub>3</sub>O<sub>4</sub>@Au NPs) [152]. Both CUR and SFN have been  
610 entrapped in the metallic NPs to improve their bioavailability and solubility. The resultant NPs were around  
611 20 nm, mono-dispersed in water, and with a high drug-loading capacity. The combined CUR and SFN NPs  
612 have demonstrated an enhanced synergistic antitumor effect in SK-BR-3 cells when compared to free CUR

613 and free SFN. The nanodelivery systems can increase therapeutic effects of SFN and CUR by apoptosis and  
614 necrosis induction as well as inhibiting migration in SK-BR-3 cells. The CUR and SFN combined NPs  
615 have been developed further using four times larger carrier NPs to increase their drug-loading capacity  
616 [153]. The resultant NPs also exhibited enhanced cytotoxicity and therapeutic effects toward MCF-7 cells.

617 Soni and Kohli have reported sulforaphane-loaded gold nanoparticles (SFN-GNPs) as a potential  
618 nanomedicine against solid tumors [154]. The size of SFN-GNPs has been optimized by four-factor  
619 three-level Box-Behnken experimental design. The optimized SFN-GNPs had a spherical shape with an  
620 average particle size of  $147.23 \pm 5.321$  nm, the zeta potential of  $-12.7 \pm 1.73$  mV, EE value of  $83.17 \pm 3.14\%$   
621 and drug loading of  $37.26 \pm 2.33\%$ . The SFN-GNPs have demonstrated enhanced retention at tumor sites as  
622 well as significant inhibition of tumor growth as compared to free SFN. In another study, Krug *et al.*  
623 synthesized sulforaphane-modified selenium nanoparticles in a simple aqueous-phase redox reaction  
624 through reduction of selenite with ascorbic acid [155], with the SFN presence on the selenium NP surface  
625 forming an adlayer. The cytotoxicity, biodistribution and excretion of resultant conjugate NPs have been  
626 investigated *in vivo* on male Wistar rats. The results suggest conjugated NPs did not induce observable  
627 negative symptoms in the rats. After 24 h, about 46% of the administered NPs were eliminated from the  
628 body in urine and feces, with the remainder mainly accumulated in the liver. The results from *in vitro*  
629 cytotoxicity assays suggested that SFN-conjugated NPs have considerable anti-cancer activity as well as  
630 selectivity toward cancer cells, which could be beneficial for the cancer treatment.

631 Mielczarek *et al.*, have evaluated a novel combination of SFN and doxorubicin entrapped in nanosized  
632 liposomes [81]. The SFN and DOX nanoliposomes were quickly taken up by MDA-MB-231 cells,  
633 followed by the release of the drug combination from the lysosomes. The *in vitro* interaction analysis using  
634 the Chou-Talalay approach suggested a high synergistic activity had been achieved by the drug  
635 combination, which enabled a favorable reduction in cytostatic dosage and an increase in cancer treatment  
636 efficiency.

637 Lu *et al.*, have built a multifunctional nanosystem based on SFN-conjugated carbon dots (SFN-CDs) for  
638 targeted imaging and inhibiting of EGFR-overexpressing cancer cells [156]. The SFN-CDs are synthesized  
639 by grafting SFN onto the amino-rich yellow fluorescent carbon dots. The obtained SFN-CDs have an  
640 average size of 5.33 nm. The *in vitro* toxicity experiments demonstrated that the SFN-CDs could  
641 significantly inhibit the proliferation of EGFR-overexpressing A549 lung cancer cell compared to  
642 BEAS-2B normal lung cells. As a result, SFN-CDs can be used as a potential nanodelivery system for both  
643 diagnostic and therapeutic functions in cancer management.

644 A recent study performed by Xu *et al.*, utilized a novel combination of CDDP and SFN encapsulated in  
645 mPEG-PLGA polymersome [157]. The CDDP was modified with poly ( $\gamma$ -L-glutamic acid) ( $\gamma$ -PGA)  
646 to produce a water-soluble CDDP derivative. SFN was encapsulated in the outer layer of polymersome  
647 which could be used to achieve an efficient glutathione (GSH) depletion, to improve the accumulation of  
648 CDDP in cancer cells. The CDDP and SFN combined NPs were more effectively internalized and could  
649 significantly reduce GSH content in breast cancer cells as compared to the free drugs, which resulted in a  
650 significant increase in DNA damage-induced apoptosis. Moreover, in an orthotopic breast cancer model,  
651 the nanoparticles achieved a significantly higher tumor accumulation and exhibited a more powerful  
652 antitumor activity. Overall, this SFN-based nanodelivery system holds great potential to enhance the  
653 sensitivity and therapeutic efficacy of Pt-based chemotherapy.

654 In summary, natural ITCs are not only the important anti-cancer therapeutic candidates but also can  
655 interact with other chemotherapies and phytochemicals to achieve synergistic antitumor effects. All above  
656 that different materials and forms of nanodelivery systems have many positive effects on ITCs biomedical  
657 applications. Nanoformulations could significantly improve the solubility, stability, and bioavailability of  
658 native ITCs, as well as minimizing their shortcomings (adverse effects). The anti-cancer nanodelivery  
659 system of natural ITCs is summarized in Table 2.

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660 Table 2. A summary of nanodelivery system for natural isothiocyanates

Type	Isothiocyanates	Carrier	Preparation method	Size(nm)	Encapsulation efficiency (EE)/Drug loading (DL) (%)	Cancer type	<i>In vitro/In vivo</i> model	Ref.
Micelle	AITC	mineral oil/Tween 80/Span 80 zein/caseinate	Emulsion inversion point (EIP) method self-assembling liquid-liquid process	137–215 nm	/	/	/	[116]
Polymeric nanoparticle	AITC	PLGA	Emulsion-solvent evaporation	200 ± 3 nm	EE 65.8% DL 24.9%	Cervical cancer Breast cancer	HeLa, MDA-MB-231 and ARPE cells	[117]
Polymeric nanoparticle	AITC	PLGA	Emulsion-solvent evaporation	200 nm	/	Cervical cancer Skin cancer	HeLa and A431 cells	[118]
Quantum dot	AITC	silicon quantum dots	Reacting the hydrogen terminated SiQDs with allyl bromide and then potassium thiocyanate	4nm		Liver cancer	HepG2 cells	[119]
Nanoemulsion	AITC	alkali-treated gelatin, polysaccharides and κ-carrageenan	Oil-in-water microemulsion	9.5 ± 0.3 nm	/	Bladder cancer	HT1376 and RAW 264.7 cells	[121]
Nanoemulsion	BITC	medium-chain	self-emulsification	242 ± 3 nm	EE 77%	Colon cancer	Caco-2, SKOV-3,	[125]

		triglycerides/ Tween 80: Transcutol flaxseed oil/egg PC	homogenization– sonication	117 ± 27 nm	EE 70%	Ovarian cancer Lung cancer	A549 cells	
Nanoemulsion	BITC	lemon oil + miglyl 812	Ultrasonication assisted cavitation	44.13 ± 3.22 nm	EE 99%	Breast cancer	MDA-MB 231	[126]
Metallic nanoparticle	BITC	cerium oxide	Ultrasonic nanoemulsion and then drug loading by incubation	5.1 ± 0.8 nm	EE 89.06 ± 2.3% DL 19.80 ± 1.54%	/	/	[129]
Nanoemulsion	BITC	rhamnolipid:Tween -80:miglyol-812:PE G200	Heating stirring-sonication method with GRAS ingredients	65.85 ± 1.34 nm	EE 99.92 ± 0.3% DL 1.26 ± 0.02%	Breast cancer	MDA MB 231 cells	[130]
Liposome	PEITC plus cisplatin	Dipalmitoylphospha tidylcholine (DSPC) and L- $\alpha$ -phosphatidylgl ycerol (EPG)	Film hydration	120-140 nm	DL ~1%	Non-small cell lung cancer	H596 cells	[137]
Liposome	PEITC	DOTMA/cholesterol /TPGS	Ethanol injection	70.0±5.8nm	/	Lung cancer	H727 cells	[139]
Nanocomposite	PEITC	graphene oxide	Drug loading by incubation	6nm	/	Liver cancer	HepG2 and 3T3 cells	[140]
Liposome	PEITC plus cisplatin	DSPC	Film hydration	173.4 ± 26.8 nm	EE 3.24 ± 0.47% DL 34.7 ± 3.2%	Non-small cell lung cancer	A549, H596, WI-38 and BEAS-2B cells	[138]
Nanosheet	PEITC plus doxorubicin	black phosphorus	Liquid exfoliation, dopamine	312 nm	/	Breast cancer	MCF-7 and MCF-7/ADR cells	[141]

Polymeric nanoparticle	SFN plus docetaxel	PLGA/hyaluronic acid	polymerization and $\pi$ - $\pi$ stacking Modified solvent-dialysis method	$179.3 \pm 2.8$ nm	DL $5.68 \pm 0.96\%$	Breast cancer	female nude mice MCF-7 cells Female Balb/c nude mice	[148]
Magnetic nanoparticle	SFN	gold-coated iron oxide nanoparticle	Co-precipitation method followed by coating with gold NPs, then drug loading by sonication and overnight incubation	$34.59 \pm 0.8$ nm	DL 56%	Breast cancer	MCF-7 cells	[149]
Micelle	SFN	mPEG-PCL	Nanoprecipitation	$\sim 118$ nm	EE $86 \pm 1.58\%$ DL $20 \pm 1.78\%$	Breast cancer	MCF-7 cells	[150]
Micelle	SFN	PCL-PEG-PCL	Nanoprecipitation	107 nm	EE $87.1 \pm 1.58\%$ DL $19.33 \pm 1.28\%$	Breast cancer	MCF-7, 4T1 and MCF10A cell Female Balb/c nude mice	[151]
Magnetic nanoparticle	SFN	PEGylated gold coated iron oxide nanoparticle	Co-precipitation method followed by coating with gold NPs, then drug loading by sonication and overnight	<30 nm	EE $72.20 \pm 0.18\%$ DL $15.74 \pm 0.015\%$	Breast cancer	SK-BR-3 cells	[152]

			incubation					
Magnetic nanoparticle	SFN plus Curcumin	PEGylated gold coated iron oxide nanoparticle	Co-precipitation method followed by coating with gold NPs, then drug loading by overnight incubation	80.57 nm	EE $81.20 \pm 0.18\%$ DL $16.74 \pm 0.015\%$	Breast cancer	MCF-7 cells Balb/c mice	[153]
Metallic nanoparticle	SFN	gold nanoparticle	Electrolysis, then drug loading by incubation	$147.23 \pm 5.321$ nm	EE $83.17 \pm 3.14\%$ DL $37.26 \pm 2.33\%$	Breast cancer Colon cancer	B16-F10, MCF-7, SW-620 and Caco-2 cells Male mice	[154]
Solid nanoparticle	SFN	selenium nanoparticle	Nanoprecipitation	$80.2 \pm 18.6$ nm	DL 2.5%	Breast cancer Colon cancer Prostate cancer	MCF-7, Caco-2, HT-29, PC-3, MCF-10A and CRL-1790 cells	[155]
Liposome	SFN plus doxorubicin	1,2-dimyristoyl-sn-glycero-3-phosphocholine (DMPC)	Film hydration	$115 \pm 8$ nm	487.5 mg/g	Breast cancer	MDA-MB-231 and MCF-7 cells	[81]
Carbon dot	SFN	carbon dot	Hydrothermal synthesis, then drug loading by conjugation	5.33 nm	/	Lung cancer	A549 and BEAS-2B cells	[156]
Polymersome	SFN plus CDDP	mPEG-PLGA	Double emulsion	$\sim 98.2$ nm	EE $58.7 \pm 4.5\%$	Breast cancer Liver cancer	MCF-7 and HepG2 cells BALB/c nude mice	[157]

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## 6 Therapeutic advantages of nanodelivery systems

Nanotechnology has been widely used in the development of new strategies for cancer management. It is playing an important role in providing both diagnostics and therapeutics for cancer. Nanodelivery systems have several therapeutic advantages over conventional administration of therapeutic agents including: an increased half-life, extended circulation time in the human body, enhanced penetration to the disease site, and improved pharmacokinetic clearance [158]. A successful nanodelivery system can be characterized by optimized encapsulation and drug loading features, sustained release of therapeutic agent at the delivery site, long storage life, and high therapeutic efficacy with no or minimized side effects [159]. In this review there are a number of featured nanodelivery system have been developed for delivery of natural ITCs as potential anti-cancer therapies. There are both solid systems such as quantum dots, carbon dots, and metallic and magnetic nanoparticles, as well as liquid systems such as liposomes, nanoemulsions, and polymersomes. Compared to the traditional forms of ITC administration, nanoparticle delivery systems offer many advantages in terms of cancer prevention and therapeutics which are described in more detail in subsections below.

### 6.1 Increase solubility and bioavailability

Several research groups have developed polymeric systems to encapsulate AITC and SFN [117, 118, 148, 150, 157]. Nanodelivery systems are formed by amphiphilic PLGA or PCL consisting of both hydrophilic and hydrophobic monomers, which self-assemble into a spherical structure in aqueous solution. ITCs are either dispersed into the polymer matrix or encapsulated in polymer. The resultant NPs are in the range of 100-200 nm with good drug loading capacities. Oil-in-water nanoemulsion has also been used to increase solubility and bioavailability of AITC and BITC [121, 125, 126, 130]. The obtained droplet size fall in the range of 10-250 nm and an encapsulation efficiency of 99% has been achieved using this nanodelivery method. Liposomes are another highly versatile nanodelivery system widely used in cancer treatment. Nanoliposomes represents nanosized self-assembled lipid vesicles which consist of phospholipid bilayers entrapping one or more therapeutic agents. The solubility and bioavailability PEITC have been significantly improved by this method [137, 138].

### 6.2 Enhanced stability

Another major advantage that nanotechnology offers is the ability to improve the stability of therapeutic agents which are sensitive, for example, to light, temperature, or pH. ITCs can be absorbed or conjugated onto the surface of a solid NP, which provides a strong scaffold to support them. They can also be encapsulated inside a NP, or dissolved within the NP matrix, which can shield them from degradation and protect them from a critical environment thus enhancing their potential pharmaceutical properties. ITC nanodelivery systems are reported to have low polydispersity and good colloidal stability that can last for several weeks [116, 117]. For example, AITC NPs have been reported to be stable when heated up to 110 °C and could also withstand three freeze-thawing cycles [121]. BITC NPs showed good long-term stability in a physiological environment and at a range of pH [125, 130]. Notably, most ITC NPs are stable at physiological conditions (pH 7.4), but release ITCs readily under acidic conditions, and thus they can be more efficiently made available in cancerous cell environments [152].

### 700 6.3 Improved tumor targeting

701 Due to the leaky vasculature of the tumor tissue, long-circulating NPs can accumulate more readily at  
702 tumor sites than in normal tissues [160]. Meanwhile, impaired lymphatic drainage also hinders NPs  
703 excretion from tumor tissue, resulting in further enhancement of NP accumulation in tumor tissues [161].  
704 This is called the enhanced permeability and retention (EPR) effect [162], which has now been widely  
705 applied in the design of NP based drug delivery system for cancer treatment. EPR is widely considered to  
706 be a major driving force for NPs to reach and accumulate in the tumor tissue, through either passive or  
707 active targeting [163]. In general, EPR is most effective with NPs in the size range of 20-200 nm, which are  
708 more likely to show improved tumor targeting. Notably, the penetration of NPs in tumors depends on the  
709 size of the NP. The smaller the size of the NP, the greater the penetration throughout the tumor. It has been  
710 demonstrated that 100 nm NPs remain close to vasculature whereas 20 nm NPs distribute throughout the  
711 tumor [164]. Moreover, NP uptake based on EPR may also vary depending on the type of tumors [165,  
712 166]. Most of the lipid nanodelivery systems developed for ITCs such as polymeric NP, micelle and  
713 liposome, range in size from 100 nm to 200 nm, and thus have enhanced tumor accumulation, resulting in  
714 significantly improved anti-cancer efficacy with minimized side effects, e.g. SFN loaded PLGA NP [148,  
715 157].

### 716 6.4 Minimize the risk of hormesis

717 In toxicology, hormesis is defined as a biphasic dose response to an exogenous or endogenous stimuli with  
718 low dose stimulation and high dose inhibition. Many drugs have been reported to exhibit such contradictory  
719 effects, also known as “biphasic dose responses” [167], which has shown significance in establishing the  
720 modality of a drug. Several studies have reported that ITCs kill cancer cells at high doses but promote  
721 cancer cell proliferation and survival at low doses [168-170]. Thus, it is crucial to optimize the anti-cancer  
722 effects and minimize the potential risks of ITCs in cancer prevention and treatment. NP based delivery  
723 systems featuring targeted delivery of ITCs could achieve high dose ITC accumulation at tumor sites,  
724 which can eliminate the unfavorable low dose stimulation effect in cancer treatments [119].

### 725 6.5 Combinational therapy

726 Simultaneous delivery of different therapeutic agents to the same tumor cells are known as co-delivery  
727 systems [171]. Such co-delivery systems could be easily achieved using recently developed  
728 nanotechnology. By the inclusion of extra components such as targeting motifs and imaging probes, an  
729 efficient multifunctional nanodelivery system could then be formed. Several combined nanodelivery  
730 systems have been developed so far incorporating ITCs and other phytochemicals e.g., curcumin or  
731 chemotherapeutics, e.g., CDDP in a single system. Combined SFN and CUR NPs showed significantly  
732 increased therapeutic effects toward breast cancer cells [153]. Combined SFN and DTX NPs  
733 simultaneously targeting DBCCs and BCSCs exhibited significantly improved antitumor efficacy  
734 compared to free drugs [148]. Encapsulating both SFN and DOX in nanoliposomes resulted in high  
735 synergistic activity towards triple negative breast cancer cells [81]. Co-delivery of SFN and CDDP by  
736 PLGA NPs largely improved the accumulation of CDDP at tumor tissue, which resulted in more powerful  
737 anti-tumor activity.

738 In summary, the application of nanotechnology in delivery of ITCs for the prevention and treatment of  
739 cancer could efficiently improve aqueous solubility and bioavailability of ITCs, extend their shelf life,

740 enhance the therapeutic efficacy by promoting their accumulation in tumors, and additionally have the  
741 advantage of eliminating hormetic effects. At the same time, combinational therapy of ITCs with other  
742 antitumor agents can also be achieved by these nanodelivery systems which can demonstrate synergistic  
743 effects on cancer treatment.

## 744 7 Conclusions and future perspectives

745 Cancer is one of the most common worldwide public health problems [24] and is in the world's top ten  
746 diseases which seriously affect human physical health. More than half of the anti-cancer drugs in clinical  
747 use are natural products or their derivatives [172] and many are plant-derived phytochemicals. Over two  
748 decades, natural ITCs from vegetables have attracted extensive research interest for cancer prevention and  
749 treatment. Many studies have confirmed that ITCs have significant antioxidant, anti-inflammatory and  
750 anti-cancer effects *in vivo* and *in vitro*. However, the epidemiological evidence regarding the consumption  
751 of dietary ITCs as chemopreventive agents have been inconsistent, which presumably due to the hormetic  
752 effect of ITCs where high doses kill cancer cells, but low doses promote cancer cell proliferation. Apart  
753 from the aforementioned, low solubility, low bioavailability, low stability and short shelf lives; there are  
754 other factors which impede the clinical use of ITCs. The application of nanotechnology provides a new idea  
755 for further development and utilization of ITCs. Current research progress suggests that nanoformulation of  
756 ITCs can improve their solubility, enhance bioavailability, provide protection against degradation, and  
757 achieve controlled and targeted release of ITCs at tumor sites.

758 One important challenge in future design of ITC nanodelivery systems is in the development of novel  
759 multifunctional nanomaterials that possess properties allowing them to deliver therapeutics across  
760 biological barriers and able to target specific types of tumor tissues in the body. Most of the studies took a  
761 passive nanodelivery approach controlled by the phenomenon of EPR. Only a few studies utilized targeting  
762 ligands, also known as 'active targeting,' to selectively deliver ITCs to tumor sites through ligand-receptor  
763 interactions. In the active delivery mode, certain RNAs, peptides, carbohydrates, and small metabolite  
764 molecules could be used as biomarkers to reach particular target sites [173]. In addition, stimuli-responsive  
765 components that can be triggered by specific stimuli (e.g., temperature, pH, or enzymes) could also be  
766 incorporated into the nanodelivery system to achieve the controlled release of the therapeutic agents at  
767 targeted sites [174]. Apart from surface features, particle size is also an important parameter of NPs which  
768 determine its pharmacokinetics, cell entry route, and interaction with the immune system [175]. In this  
769 review, we found that the size of ITC NPs varied from 4 nm up to over 300 nm. In principle, NPs in the  
770 size range of 20-200 nm can be delivered to the tumor site through the EPR effect. However, the *in vivo*  
771 delivery of NPs also depends on the types of tumor and their local conditions [165, 166]. Tumors with  
772 increased interstitial fluid pressure (IFP) are harder to permeate by passive targeting. It is also reported that  
773 the smaller the size of NP, the greater the penetration throughout the tumor. NPs with a mean size less than  
774 100 nm are ideal for even distribution throughout the tumor. Thus, special attention should be paid to  
775 control the NP size for efficient drug delivery. Most of the reported studies lack *in vivo* evaluation of the  
776 pharmacokinetic and pharmacodynamic properties of ITC NPs. So far, none of the ITC nanodelivery  
777 systems have proceeded into the clinical trials, which suggests more preclinical work is needed to verify the  
778 safety and efficacy of nano formulated ITCs as a new cancer therapy.

779

780

781 **Acknowledgments**

782 The study is funded by the Cancer Prevention Research Trust UK. We thank Mr James Bacon, Dr Peimeng  
783 Wei and Dr Samuel Atkinson for critical reading of this review article.

784 The authors declare no conflict of interest.

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786 **References**

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### **Highlights**

- Natural isothiocyanates show significant antioxidant, anti-inflammatory and anti-cancer activities.
- Nano-formulation enhances delivery of isothiocyanates in cancer therapy.
- Combination of isothiocyanates and anti-cancer drugs exhibit synergistic therapeutic potential.

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